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56 evolved from MitoEAGLE Working Group 57 Meetings and a bottom-up spirit of COST in 58 phase 1: This is an open invitation to 59 scientists and students to join as co-authors, to provide a balanced view on mitochondrial 60 respiratory control, fundamental 61 а introductory presentation of the concept of 62 63 the protonmotive force, and a consensus 64 statement on reporting data of mitochondrial

respiration in terms of metabolic flows and



Mitochondrial fitness mapping - Quality management network

fluxes. We plan a series of follow-up reports by the expanding MitoEAGLE Network, to increase
the scope of recommendations on harmonization and facilitate global communication and
collaboration.

69 Phase 2 - until October 12: We continue to invite comments and suggestions on the 70 MitoEAGLE preprint, particularly if you are an early career investigator adding an open 71 future-oriented perspective, or an established scientist providing a balanced historical basis. 72 Your critical input into the quality of the manuscript will be most welcome, improving our aims 73 to be educational, general, consensus-oriented, and practically helpful for students working in 74 mitochondrial respiratory physiology.

To join as a co-author, please feel free to focus on a particular section in terms of direct
input and references, contributing to the scope of the manuscript from the perspective of your
expertise. Your comments will be largely posted on the discussion page of the MitoEAGLE
preprint website.

If you prefer to submit comments in the format of a referee's evaluation rather than a
contribution as a co-author, I will be glad to distribute your views to the updated list of coauthors for a balanced response. We would ask for your consent on this open bottom-up policy.
We organize a MitoEAGLE session linked to our series of reports at the MiPconference

- 83 Nov 2017 in Hradec Kralove in close association with the MiPsociety (where you hopefully will
- 84 *attend) and at EBEC 2018 in Budapest.*

» http://www.mitoeagle.org/index.php/MiP2017\_Hradec\_Kralove\_CZ

85 86

- 87 *I thank you in advance for your feedback.*
- 88 With best wishes,
- 89
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142 Abstract

143 Clarity of concept and consistency of nomenclature are key trademarks of a research field. These trademarks facilitate effective transdisciplinary communication, education, and 144 ultimately further discovery. As the knowledge base and importance of mitochondrial 145 146 physiology to human health expand, the necessity for harmonizing nomenclature concerning 147 mitochondrial respiratory states and rates has become increasingly apparent. Peter Mitchell's 148 concept of the protonmotive force establishes the links between electrical and chemical 149 components of energy transformation and coupling in oxidative phosphorylation. This unifying 150 concept provides the framework for developing a consistent nomenclature for mitochondrial 151 physiology and bioenergetics. Herein, we follow IUPAC guidelines on general terms of 152 physical chemistry, extended by the concepts of open systems and irreversible thermodynamics. 153 We align the nomenclature of classical bioenergetics on respiratory states with a concept-driven 154 constructive terminology to address the meaning of each respiratory state. Furthermore, we 155 suggest uniform standards for the evaluation of respiratory states that will ultimately support 156 the development of databases of mitochondrial respiratory function in species, tissues and cells 157 studied under diverse physiological and experimental conditions. In this position statement, in 158 the frame of COST Action CA15203 MitoEAGLE, we endeavour to provide a balanced view 159 on mitochondrial respiratory control, a fundamental introductory presentation of the concept of 160 the protonmotive force, and a critical discussion on reporting data of mitochondrial respiration 161 in terms of metabolic flows and fluxes.

162

*Keywords:* Mitochondrial respiratory control, coupling control, mitochondrial
preparations, protonmotive force, chemiosmotic theory, oxidative phosphorylation, OXPHOS,
efficiency, electron transfer, ET; proton leak, LEAK, residual oxygen consumption, ROX, State
2, State 3, State 4, normalization, flow, flux

169 170	Box 1: * Does the public expect biologists to understand
170 171	In brief: Does the public expect biologists to understand Darwin's theory of evolution?
172	mitochondria * Do students expect that researchers of bioenergetics can explain
173	and BioblastsMitchell's theory of chemiosmotic energy transformation?
174	Mitochondria were described for the first time in 1857 by Rudolph Albert von Kölliker as
175	granular structures or 'sarkosomes'. In 1886 Richard Altman called them 'bioblasts' (published
176	1894). The word 'mitochondrium' (Greek mitos: thread; chondros: granule) was introduced by
177	Carl Benda (1898). Mitochondria are the oxygen consuming electrochemical generators which
178	evolved from endosymbiotic bacteria (Margulis 1970). The bioblasts of Richard Altmann
179	(1894) include not only the mitochondria, but also symbiotic and free-living bacteria. We now
180	recognize mitochondria as dynamic organelles with a double membrane that are contained
181	within eukaryotic cells. The inner mitochondrial membrane shows dynamic tubular and disk-
182	shaped cristae that separate the mitochondrial matrix, <i>i.e.</i> the internal mitochondrial
183	compartment, and the intermembrane space; the latter being enclosed by the outer
184	mitochondrial membrane. Mitochondria are the structural and functional elemental units of cell
185	respiration, where cell respiration is defined as the consumption of oxygen coupled to
186	electrochemical proton translocation across the inner mitochondrial membrane. In the process
187	of oxidative phosphorylation (OXPHOS), the reduction of $O_2$ is electrochemically coupled to
188	the transformation of energy in the form of ATP (Mitchell 2011). These powerhouses of the
189	cell contain the machinery of the OXPHOS pathway, including transmembrane respiratory
190	complexes ( <i>i.e.</i> FMN, Fe-S and cytochrome b, c, aa <sub>3</sub> redox systems), alternative
191	dehydrogenases and oxidases, the coenzyme ubiquinone (coenzyme Q) and ATP synthase
192	together with the enzymes of the tricarboxylic acid cycle and the fatty acid oxidation enzymes,
193	ion transporters, including substrate, co-factor and metabolite transporters as well as proton
194	pumps, and mitochondrial kinases related to energy transfer pathways. The mitochondrial
195	proteome comprises over 1,200 proteins (Mitocharta), mostly encoded by nuclear DNA

(nDNA), with a variety of functions, many of which are relatively well known (e.g. apoptosis-196 197 regulating proteins), are still under investigation, or need to be identified (alanine transporter). 198 Mitochondria typically maintain several copies of their own genome (hundred to thousands per 199 cell) which is maternally inherited and known as mitochondrial DNA (mtDNA). One exception to strictly maternal inheritance in animals is found in bivalves (Breton et al. 2007). mtDNA is 200 201 16.5 Kb in length, contains 13 protein-coding genes for subunits of the transmembrane 202 respiratory Complexes CI, CIII, CIV and ATP synthase, and also encodes 22 tRNAs and the 203 mitochondrial 16S and 12S rRNA. The mitochondrial genome is both regulated and 204 supplemented by nuclear-encoded mitochondrial targeted proteins. Evidence has accumulated 205 that additional gene content is encoded in the mitochondrial genome, e.g. microRNAs, piRNA, 206 smithRNAs, repeat associated RNA, and even additional proteins (Duarte et al. 2014; Lee et 207 al. 2015; Cobb et al. 2016). The inner mitochondrial membrane contains the non-bilayer 208 phospholipid cardiolipin, which is not present in any other eukaryotic cellular membrane. Cardiolipin promotes the formation of respiratory supercomplexes, which are supramolecular 209 210 assemblies based upon specific, though dynamic, interactions between individual respiratory 211 complexes (Greggio et al. 2017; Lenaz et al. 2017). There is a constant crosstalk between 212 mitochondria and the other cellular components at the transcriptional or post-translational level, 213 and through cell signalling in response to varying energy demands (Quiros et al. 2016). In 214 addition to mitochondrial movement along the microtubules, mitochondrial morphology can 215 change in response to energy requirements of the cell via processes known as fusion and fission 216 through which mitochondria can communicate within a network, and in various pathological 217 states which cause swelling or dysregulation of fission and fusion. Mitochondrial dysfunction 218 is associated with a wide variety of genetic and degenerative diseases. Therefore, a better 219 understanding of mitochondrial physiology will improve our understanding of the etiology of 220 disease and the diagnostic repertoire of mitochondrial medicine. Abbreviation: mt, as generally 221 used in mtDNA. Mitochondrion is singular and mitochondria is plural.

222 'For the physiologist, mitochondria afforded the first opportunity for an experimental
223 approach to structure-function relationships, in particular those involved in active transport,
224 vectorial metabolism, and metabolic control mechanisms on a subcellular level' (Ernster and
225 Schatz 1981).

226

#### 227 **1. Introduction**

228 Mitochondria are the powerhouses of the cell with numerous physiological, molecular, 229 and genetic functions (Box 1). Every study of mitochondrial function and disease is faced with Evolution, Age, Gender and sex, Lifestyle, and Environment (EAGLE) as essential background 230 231 conditions intrinsic to the individual patient or subject, cohort, species, tissue and to some extent 232 even cell line. As a large and highly coordinated group of laboratories and researchers, the 233 mission of the global MitoEAGLE Network is to generate the necessary scale, type, and quality 234 of consistent data sets and conditions to address this intrinsic complexity. Harmonization of experimental protocols and implementation of a quality control and data management system 235 236 is required to interrelate results gathered across a spectrum of studies and to generate a 237 rigorously monitored database focused on mitochondrial respiratory function. In this way, researchers within the same and across different disciplines will be positioned to compare their 238 239 findings to an agreed upon set of clearly defined and accepted international standards.

240 Reliability and comparability of quantitative results depend on the accuracy of measurements under strictly-defined conditions. A conceptually clearly-defined framework is 241 also required to warrant meaningful interpretation and comparability of experimental outcomes 242 243 carried out by research groups at different institutes. With an emphasis on quality of research, collected data can be useful far beyond the specific question of a specific experiment. Vague or 244 245 ambiguous jargon can lead to confusion and may relegate valuable signals to wasteful noise. For this reason, measured values must be expressed in standardized units for each parameter 246 used to define mitochondrial respiratory function. Standardization of nomenclature and 247

technical terms is essential to improve the awareness of the intricate meaning of divergent scientific vocabulary. The focus on coupling states, the protonmotive force and fluxes through metabolic pathways of aerobic energy transformation in mitochondrial preparations is a first step in the attempt to generate a harmonized and conceptually oriented nomenclature in bioenergetics and mitochondrial physiology. Coupling states of intact cells and respiratory control by fuel substrates and specific inhibitors of respiratory enzymes will be reviewed in subsequent communications.

255

256

#### **2. Respiratory coupling states in mitochondrial preparations**

257 'Every professional group develops its own technical jargon for talking about
258 matters of critical concern ... People who know a word can share that idea with
259 other members of their group, and a shared vocabulary is part of the glue that holds
260 people together and allows them to create a shared culture' (Miller 1991).

261

Mitochondrial preparations are defined as either isolated mitochondria, or tissue and 262 263 cellular preparations in which the barrier function of the plasma membrane is disrupted. The 264 plasma membrane separates the cytosol, nucleus and organelles (the intracellular compartment) 265 from the environment of the cell. The plasma membrane consists of a lipid bilayer, embedded 266 proteins and attached organic molecules which collectively control the selective permeability 267 of ions, organic molecules and particles across the cell boundary. The intact plasma membrane, 268 therefore, prevents the passage of many water-soluble mitochondrial substrates, such as 269 succinate or ADP, that are required for the analysis of respiratory capacity at kinetically 270 saturating concentrations, thus limiting the scope of investigations into mitochondrial 271 respiratory function in intact cells. The cholesterol content of the plasma membrane is high 272 compared to mitochondrial membranes. Therefore, mild detergents, such as digitonin and 273 saponin, can be applied to selectively permeabilize the plasma membrane by interaction with

cholesterol and allow free exchange of cytosolic components with ions and organic molecules 274 275 of the immediate cell environment, while maintaining the integrity and localization of 276 organelles, cytoskeleton and the nucleus. Application of optimum concentrations of these mild 277 detergents leads to the complete loss of cell viability, tested by nuclear staining, while 278 mitochondrial function remains unaffected, as shown by an unaltered respiration rate of 279 mitochondria after the addition of such low concertations of digitonin and saponin. In addition 280 to mechanical permeabilization during homogenization of fresh tissue, saponin may be applied 281 to ensure permeabilization of all cells. Crude homogenate and cells permeabilized in the 282 respiration chamber contain all components of the cell at highly diluted concentrations. All 283 mitochondria are retained in chemically permeabilized mitochondrial preparations and crude 284 tissue homogenates. In the preparation of isolated mitochondria, the cells or tissues are 285 homogenized, and the mitochondria are separated from other cell fractions and purified by 286 centrifugation, entailing the loss of a significant fraction of mitochondria. The term 287 mitochondrial preparation does not include further fractionation of mitochondrial components, 288 as well as submitochondrial particles.

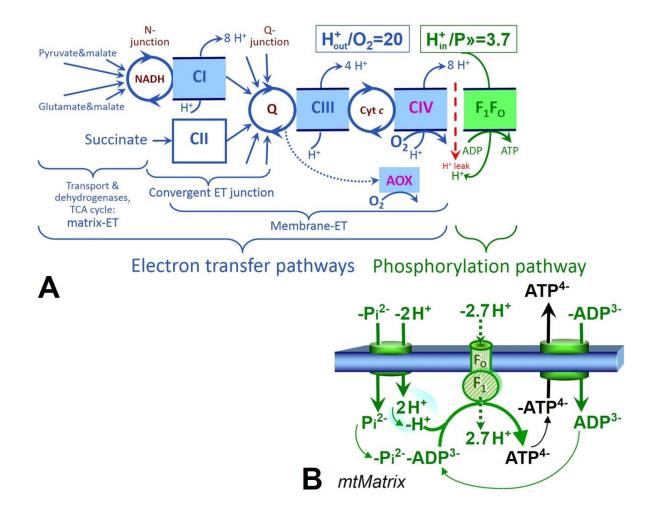
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### 290 2.1. Three coupling states of mitochondrial preparations and residual oxygen consumption

291 Coupling control states: To extend the classical nomenclature on mitochondrial 292 coupling states (Section 2.4) by a concept-driven terminology that incorporates explicit 293 information on the nature of the respiratory states, the terminology must be general and not 294 restricted to any particular experimental protocol or mitochondrial preparation (Gnaiger 2009). 295 We focus primarily on the conceptual 'why', along with clarification of the experimental 'how'. 296 In the following section, the concept-driven terminology is explained and coupling states are 297 defined. To provide a diagnostic reference for respiratory capacities of core energy metabolism, the capacity of oxidative phosphorylation, OXPHOS, is measured at kinetically saturating 298 concentrations of ADP and inorganic phosphate, Pi. The oxidative capacity of the electron 299

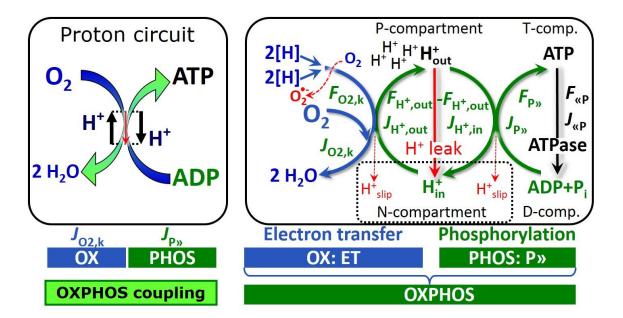
300 transfer-pathway, ET-pathway, reveals the limitation of OXPHOS capacity mediated by the 301 phosphorylation pathway. The ET and phosphorylation pathways comprise coupled segments 302 of the OXPHOS pathway. ET capacity is measured as noncoupled respiration by application of 303 external uncouplers. The contribution of intrinsically uncoupled oxygen consumption is most 304 easily studied by not stimulating or arresting phosphorylation, when oxygen consumption 305 compensates mainly for the proton leak; the corresponding states are collectively classified as 306 LEAK states (Table 1). Fuel substrates and ET inhibitors are kept constant, *i.e.* maintaining a 307 defined ET-pathway state, while (1) adding ADP or P<sub>i</sub>, (2) inhibiting the phosphorylation 308 pathway, and (3) performing uncoupler titrations to induce different coupling states (Fig. 1).

309 Respiratory capacities and kinetic control: Coupling control states are established in 310 the study of mitochondrial preparations to obtain reference values for various output variables. 311 Physiological conditions in vivo may deviate substantially from these experimentally obtained 312 states. Since kinetically saturating concentrations, e.g. of ADP or oxygen, may not apply to physiological intracellular conditions, relevant information is obtained in studies of kinetic 313 314 responses to conditions intermediate between the LEAK state at zero [ADP] and the OXPHOS 315 state at saturating [ADP], or of respiratory capacities in the range between kinetically saturating 316 [O<sub>2</sub>] and anoxia (Gnaiger 2001). We define respiratory capacities, comparable to channel 317 capacity in information theory, as the upper bound of the rate of respiration measured in defined coupling and pathway control states of mitochondrial preparations. 318



320

321 Fig. 1. The oxidative phosphorylation pathway, OXPHOS pathway. (A) Electron transfer, ET, 322 coupled to phosphorylation. Multiple convergent electron transfer pathways are shown from NADH and 323 succinate; additional arrows indicate electron entry through electron transferring flavoprotein, 324 glycerophosphate dehydrogenase, dihydro-orotate dehydrogenase, choline dehydrogenase, and 325 sulfide-ubiquinone oxidoreductase. The branched pathway of oxygen consumption by alternative quinol 326 oxidase (AOX) is indicated by the dotted arrow. H<sup>+</sup>out/O<sub>2</sub> is the ratio of outward proton flux from the matrix 327 space to catabolic O<sub>2</sub> flux in the NADH-linked pathway. H<sup>+</sup><sub>in</sub>/P<sup>»</sup> is the ratio of inward proton flux from the 328 inter-membrane space to the flux of phosphorylation of ADP to ATP. Due to proton leak and slip these 329 are not fixed stoichiometries. (B) Phosphorylation pathway catalyzed by the  $F_1F_0$  ATP synthase, 330 adenine nucleotide translocase, and inorganic phosphate transporter. The H+in/P » stoichiometry is the sum of the coupling stoichiometry in the ATP synthase reaction (-2.7 H<sup>+</sup> from the intermembrane space, 331 2.7 H<sup>+</sup> to the matrix) and the proton balance in the translocation of ADP<sup>2-</sup>, ATP<sup>3-</sup> and Pi<sup>2-</sup>. See Eqs. 3 332 and 4 for further explanation. Modified from (A) Lemieux et al. (2017) and (B) Gnaiger (2014). 333



335

336 Fig. 2. The proton circuit and coupling in oxidative phosphorylation (OXPHOS). Oxygen flux, Jo2,k, 337 through the catabolic electron transfer (ET) pathway k is coupled to flux through the phosphorylation 338 pathway of ADP to ATP, J<sub>P\*</sub>, by the proton pumps of the ET-pathway, pushing the outward proton flux, 339  $J_{H+,out}$ , and generating the output protonmotive force,  $F_{H+,out}$ . ATP synthase is coupled to inward proton 340 flux,  $J_{H+,in}$ , to phosphorylate ADP with inorganic phosphate to ATP, driven by the input protonmotive 341 force,  $F_{H+,in}$ =- $F_{H+,out}$ . 2[H] indicates the reduced hydrogen equivalents of fuel substrates that provide the 342 chemical input force,  $F_{O2,k}$  [kJ/mol O<sub>2</sub>], of the catabolic reaction k with oxygen (Gibbs energy of reaction 343 per mole O<sub>2</sub> consumed in reaction k), typically in the range of -460 to -480 kJ/mol. The output force is 344 given by the phosphorylation potential difference (ADP phosphorylated to ATP), F<sub>P</sub>, which varies in vivo 345 ranging from about 48 to 62 kJ/mol under physiological conditions. Fluxes,  $J_{B}$ , and forces,  $F_{B}$ , are 346 expressed in either chemical units, [mol·s<sup>-1</sup>·m<sup>-3</sup>] and [J·mol<sup>-1</sup>] respectively, or electrical units, [C·s<sup>-1</sup>·m<sup>-3</sup>] 347 and  $[J \cdot C^{-1}]$  respectively, per volume,  $V[m^3]$ , of the system. The system defined by the boundaries shown 348 as a full black line is not a black box, but is analysed as a compartmental system. The negative 349 compartment (N-compartment, enclosed by the dotted line) is the matrix space, separated from the 350 positive compartment (P-compartment) by the inner mitochondrial membrane. ADP+Pi and ATP are the 351 substrate- and product-compartments (scalar D- and T-comp.), respectively. Chemical potentials of all 352 substrates and products involved in the scalar reactions are measured in the P-compartment for 353 calculation of the scalar forces  $F_{O2,k}$  and  $F_{P,*}=-F_{*P}$  (**Box 2**). Modified from Gnaiger (2014).

355 **Phosphorylation**, **P»**: *Phosphorylation* in the context of OXPHOS is defined as 356 phosphorylation of ADP to ATP. On the other hand, the term phosphorylation is used generally 357 in many different contexts, e.g. protein phosphorylation. This justifies consideration of a 358 symbol more discriminating and specific than P as used in the P/O ratio (phosphate to atomic oxygen ratio), where P indicates phosphorylation of ADP to ATP or GDP to GTP. We propose 359 360 the symbol P» for the endergonic direction of phosphorylation ADP $\rightarrow$ ATP, and likewise the 361 symbol «P for the corresponding exergonic hydrolysis ATP→ADP (Fig. 2; Box 3). ATP 362 synthase is the proton pump of the phosphorylation pathway (Fig. 1B). P» may also involve 363 substrate-level phosphorylation as part of the tricarboxylic acid cycle (succinyl-CoA ligase) and phosphorylation of ADP catalyzed by phosphoenolpyruvate carboxykinase, adenylate 364 365 kinase, creatine kinase, hexokinase and nucleoside diphosphate kinase (NDPK). Kinase cycles 366 are involved in intracellular energy transfer and signal transduction for regulation of energy flux. In isolated mammalian mitochondria ATP production catalyzed by adenylate kinase, 367 2ADP ↔ ATP + AMP, proceeds without fuel substrates in the presence of ADP (Komlódi and 368 369 Tretter 2017).  $J_{P*}/J_{O2,k}$  (P\*/O<sub>2</sub>) is two times the 'P/O' ratio of classical bioenergetics. The 370 effective  $P \gg O_2$  ratio is diminished by: (1) the proton leak across the inner mitochondrial 371 membrane from low pH in the P-phase to high pH in the N-phase (P, positive; N, negative); (2) 372 cycling of other cations; (3) proton slip in the proton pumps when a proton effectively is not pumped; and (4) electron leak in the univalent reduction of oxygen (O<sub>2</sub>; dioxygen) to superoxide 373 374 anion radical  $(O_2^{\bullet})$ . 375 376 377

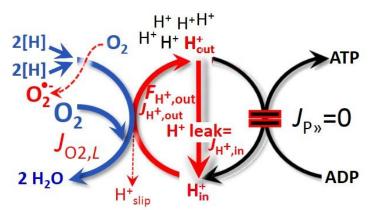
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Table 1. Coupling states and residual oxygen consumption in mitochondrial preparations in relation to respiration and phosphorylation rate,  $J_{O2,k}$  and  $J_{P,v}$ , and protonmotive force,  $F_{H+,out}$ . Coupling states are established at kinetically saturating concentrations of fuel substrates and O<sub>2</sub>.

State	J <sub>O2,k</sub>	$J_{\mathrm{P}*}$	F <sub>H+,out</sub>	Inducing factors	Limiting factors
LEAK	<i>L</i> ; low proton leak- dependent respiration	0	max.	Proton leak, slip, and cation cycling	$J_{P}=0: (1)$ without ADP, $L_N; (2)$ max. ATP/ADP ratio, $L_T;$ or (3) inhibition of the phosphorylation pathway, $L_{Omy}$
OXPHOS	<i>P</i> ; high ADP- stimulated respiration	max.	high	Kinetically saturating [ADP] and [P <sub>i</sub> ]	$J_{P*}$ by phosphorylation pathway; or $J_{O2,k}$ by ET-pathway capacity
ET	<i>E</i> ; max. noncoupled respiration	0	low	Optimal external uncoupler concentration for max. oxygen flux	J <sub>O2,k</sub> by ET-pathway capacity
ROX	<i>Rox</i> ; min. residual O <sub>2</sub> consumption	0	0	$J_{O2,Rox}$ in non-ET- pathway oxidation reactions	Full inhibition of ET- pathway or absence of fuel substrates

- 385 386
- 387 **LEAK state (Fig. 3**): The

388 LEAK state is defined as a state mitochondrial respiration 389 of 390 when  $O_2$ flux mainly 391 compensates for the proton leak in the absence of ATP synthesis, 392 393 kinetically at saturating 394 concentrations of  $O_2$ and respiratory substrates. LEAK 395 396 respiration is measured to obtain



**Fig. 3. LEAK state:** Phosphorylation is arrested,  $J_{P*}=0$ , and oxygen flux,  $J_{O2,L}$ , is controlled mainly by the proton leak, which equals  $J_{H+,in}$ , at maximum protonmotive force,  $F_{H+,out}$  (See also Fig. 2).

in the absence of adenylates; (2) after depletion of ADP at maximum ATP/ADP ratio; or (3) 398 399 after inhibition of the phosphorylation pathway by inhibitors of ATP synthase, such as 400 oligomycin, or adenine nucleotide translocase, such as carboxyatractyloside.

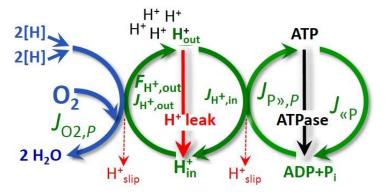
401 Proton leak: Proton leak is the *uncoupled* process in which protons are translocated 402 across the inner mitochondrial membrane in the dissipative direction of the downhill 403 protonmotive force without coupling to phosphorylation (Fig. 3). The proton leak flux depends 404 on the protonmotive force, is a property of the inner mitochondrial membrane, may be enhanced 405 due to possible contaminations by free fatty acids, and is physiologically controlled. In 406 particular, inducible uncoupling mediated by uncoupling protein 1 (UCP1) is physiologically 407 controlled, e.g., in brown adipose tissue. UCP1 is a proton channel of the inner mitochondrial 408 membrane facilitating the conductance of protons across the inner mitochondrial membrane. 409 As consequence of this effective short-circuit, the protonmotive force diminishes, resulting in 410 stimulation of electron transfer to oxygen and heat dissipation without phosphorylation of ADP. Mitochondrial injuries may lead to dyscoupling as a pathological or toxicological cause of 411 uncoupled respiration, e.g., as a consequence of opening the permeability transition pore. 412 Dyscoupled respiration is distinguished from the experimentally induced noncoupled 413 414 respiration in the ET state. Under physiological conditions, the proton leak is the dominant 415 contributor to the overall leak current.

**Proton slip:** Proton slip is the *decoupled* process in which protons are only partially 416 translocated by a proton pump of the ET-pathways and slip back to the original compartment 417 418 (Dufour et al. 1996). Proton slip can also happen in association with the ATP-synthase, in which 419 case the proton slips downhill across the membrane to the matrix without contributing to ATP 420 synthesis. In each case, proton slip is a property of the proton pump and increases with the 421 turnover rate of the pump.

422 Cation cycling: Proton leak is a leak current of protons. There can be other cation 423 contributors to leak current including calcium and probably magnesium. Calcium current is balanced by mitochondrial Na/Ca exchange, which is balanced by Na/H exchange or K/H
exchange. This is another effective uncoupling mechanism different from proton leak and slip.
Small differences of terms, *e.g.*, uncoupled, noncoupled, are easily overlooked and may
be erroneously perceived as identical. Even with an attempt at rigorous definition, the common
use of such terms may remain vague (Table 2).

429 **OXPHOS state** (**Fig. 4**):

430 The OXPHOS state is defined as 431 respiratory the state with kinetically 432 saturating 433 concentrations of O<sub>2</sub>, respiratory 434 and phosphorylation substrates, 435 and absence of exogenous uncoupler, which provides an 436 estimate of the maximal capacity 437 of OXPHOS in any given 438



**Fig. 4. OXPHOS state:** Phosphorylation,  $J_{P*}$ , is stimulated by kinetically saturating [ADP] and inorganic phosphate, [P<sub>i</sub>], and is supported by a high protonmotive force,  $F_{H+,out}$ . O<sub>2</sub> flux,  $J_{O2,P}$ , is highly coupled at a maximum P\*/O<sub>2</sub> ratio,  $J_{P*,P}/J_{O2,P}$  (See also Fig. 2).

pathway control state. Respiratory capacities at kinetically saturating substrate concentrations provide reference values or upper limits of performance, aiming at the generation of data sets for comparative purposes. Any effects of substrate kinetics are thus separated from reporting actual mitochondrial capacity for oxidation during coupled respiration, against which physiological activities can be evaluated.

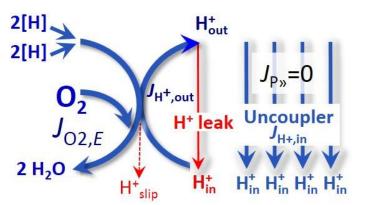
As discussed previously, 0.2 mM ADP does not fully saturate flux in isolated mitochondria (Gnaiger 2001; Puchowicz *et al.* 2004); greater ADP concentration is required, particularly in permeabilized muscle fibres and cardiomyocytes, to overcome limitations by intracellular diffusion and by the reduced conductance of the outer mitochondrial membrane (Jepihhina *et al.* 2011, Illaste *et al.* 2012, Simson *et al.* 2016) either through interaction with tubulin (Rostovtseva *et al.* 2008) or other intracellular structures (Birkedal *et al.* 2014). In 450 permeabilized muscle fibre bundles of high respiratory capacity, the apparent  $K_m$  for ADP 451 increases up to 0.5 mM (Saks *et al.* 1998), indicating that >90% saturation is reached only at 452 >5 mM ADP. Similar ADP concentrations are also required for accurate determination of 453 OXPHOS capacity in human clinical cancer samples and permeabilized cells (ref). Whereas 2.5 454 to 5 mM ADP is sufficient to obtain the actual OXPHOS capacity in many types of 455 permeabilized cell and tissue preparations, experimental validation is required in each specific 456 case.

457

Term	Respiration	<b>P</b> »/O <sub>2</sub>	Note
Fully coupled	P-L	max.	OXPHOS capacity corrected for LEAK respiration ( <b>Fig. 6</b> )
Well coupled	Р	high	Phosphorylating respiration with a variable intrinsic LEAK component ( <b>Fig. 4</b> )
Loosely coupled	up to E	low	Inducibly uncoupled by UCP1 or Ca <sup>2+</sup> cycling
Dyscoupled	Р	low	Pathologically, toxicologically, environmentally increased uncoupling, mitochondrial dysfunction
Uncoupled and decoupled	L	0	Non-phosphorylating intrinsic LEAK respiration without added protonophore ( <b>Fig. 3</b> )
Noncoupled	Ε	0	Non-phosphorylating respiration stimulated to maximum flux at optimum exogenous uncoupler concentration ( <b>Fig. 5</b> )

# 458 **Table 2. Distinction of terms related to coupling.**

460 **Electron transfer state** 461 (Fig. 5): The ET state is defined as the noncoupled state with 462 463 kinetically saturating 464 concentrations of O<sub>2</sub>, respiratory 465 substrate optimum and 466 uncoupler exogenous 467 concentration for maximum O<sub>2</sub> flux, as an estimate of oxidative 468



**Fig. 5. ET state:** Noncoupled respiration,  $J_{O2,E}$ , is maximum at optimum exogenous uncoupler concentration and phosphorylation is zero,  $J_{P}$ =0 (See also Fig. 2).

469 ET capacity. Inhibition of respiration is observed at higher than optimum uncoupler 470 concentrations. As a consequence of the nearly collapsed protonmotive force, the driving force 471 is insufficient for phosphorylation and  $J_{P,v}=0$ .

Besides the three fundamental coupling states of mitochondrial preparations, thefollowing respiratory state also is relevant to assess respiratory function:

474 ROX: Residual oxygen consumption (ROX) is defined as O<sub>2</sub> consumption due to oxidative side reactions remaining after inhibition of ET. ROX is not a coupling state but 475 476 represents a baseline that is used to correct mitochondrial respiration in defined coupling states. 477 ROX is not necessarily equivalent to non-mitochondrial respiration, considering oxygen-478 consuming reactions in mitochondria not related to ET, such as oxygen consumption in 479 reactions catalyzed by monoamine oxidases (type A and B), monooxygenases (cytochrome 480 P450 monooxygenases), dioxygenase (sulfur dioxygenase and trimethyllysine dioxygenase), several hydoxylases, and more. Mitochondrial preparations, especially those obtained from 481 482 liver, are contaminated by peroxisomes. This fact makes the exact determination of mitochondrial oxygen consumption and mitochondria-associated generation of reactive oxygen 483 species complicated (Schönfeld et al. 2009). The dependence of ROX-linked oxygen 484 485 consumption needs to be studied in detail with respect to non-ET enzyme activities, availability

486 of specific substrates, oxygen concentration, and electron leakage leading to the formation of487 reactive oxygen species.

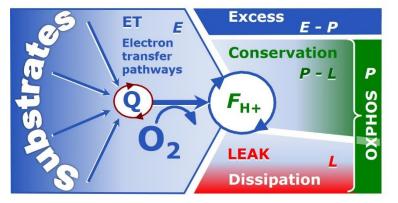
488

489 2.2. Coupling states and respiratory rates

It is important to distinguish metabolic pathways from metabolic states and the
corresponding metabolic rates; for example: electron transfer pathways (Fig. 6), ET state (Fig.
5), and ET capacity, *E*, respectively (Table 1). The protonmotive force is *high* in the OXPHOS
state when it drives phosphorylation, *maximum* in the LEAK state of coupled mitochondria,
driven by LEAK respiration at a minimum back flux of protons to the matrix side, and *very low*in the ET state when uncouplers short-circuit the proton cycle (Table 1).

496

497 Fig. 6. Four-compartment model 498 oxidative phosphorylation. of 499 Respiratory states (ET, OXPHOS, 500 LEAK) and corresponding rates (E, 501 P, L) are connected by the 502 protonmotive force, F<sub>H+,out</sub>. Electron 503 transfer capacity, E, is partitioned



into (1) dissipative LEAK respiration, *L*, when the capacity to perform work is irreversibly lost, (2) net
OXPHOS capacity, *P-L*, with partial conservation of the capacity to perform work, and (3) the excess
capacity, *E-P*. Modified from Gnaiger (2014).

507

The three coupling states, ET, LEAK and OXPHOS, are presented in a schematic context with the corresponding respiratory rates, abbreviated as *E*, *L* and *P*, respectively (**Fig. 6**). This clarifies that *E* may exceed or be equal to *P*, but *E* cannot theoretically be lower than *P*. *E*<*P* must be discounted as an artefact, which may be caused experimentally by: (1) loss of oxidative capacity during the time course of the respirometric assay, since *E* is measured subsequently to *P*; (2) using too low uncoupler concentrations; (3) using high uncoupler concentrations which

inhibit ET (Gnaiger 2008); (4) high oligomycin concentrations applied for measurement of L 514 515 before titrations of uncoupler, when oligomycin exerts an inhibitory effect on E. On the other 516 hand, the excess ET capacity is overestimated if non-saturating [P<sub>i</sub>] or [ADP] (State 3) are used. 517 E > P is observed in many types of mitochondria, varying between species, tissues and cell 518 types. It is the excess ET capacity pushing the phosphorylation pathway flux (Fig. 1B) to the 519 limit of its *capacity of utilizing* the protonmotive force. Within any type of mitochondria, the 520 magnitude of E > P depends on (1) the pathway control state with single or multiple electron 521 input into the Q-junction and involvement of three or fewer coupling sites determining the  $H^+_{out}/O_2$  coupling stoichiometry (Fig. 1A); and (2) the biochemical coupling efficiency 522 523 expressed as (E-L)/E, since an increase of L causes P to increase towards the limit of E. The 524 excess E-P capacity, E-P, therefore, provides a sensitive diagnostic indicator of specific injuries 525 of the phosphorylation pathway, under conditions when E remains constant but P declines 526 relative to controls (Fig. 6). Substrate cocktails supporting simultaneous convergent electron transfer to the Q-junction for reconstitution of tricarboxylic acid cycle (TCA cycle) function 527 528 establish pathway control states with high ET capacity, and consequently increase the 529 sensitivity of the *E*-*P* assay.

530 When subtracting L from P, the dissipative LEAK component in the OXPHOS state may 531 be overestimated. This can be avoided by measuring LEAK respiration in a state when the protonmotive force is adjusted to its slightly lower value in the OXPHOS state, e.g., by titration 532 533 of an ET inhibitor. Any turnover-dependent components of proton leak and slip, however, are 534 underestimated under these conditions (Garlid et al. 1993). In general, it is inappropriate to use 535 the term ATP production or ATP turnover for the difference of oxygen consumption measured 536 in states P and L. The difference P-L is the upper limit of the part of OXPHOS capacity that is 537 freely available for ATP production (corrected for LEAK respiration) and is fully coupled to 538 phosphorylation with a maximum mechanistic stoichiometry (Fig. 6).

540 2.3. Classical terminology for isolated mitochondria

- 541 'When a code is familiar enough, it ceases appearing like a code; one forgets that
- 542 there is a decoding mechanism. The message is identical with its meaning'
- 543 (Hofstadter 1979).

Chance and Williams (1955; 1956) introduced five classical states of mitochondrial respiration
and cytochrome redox states. Table 3 shows a protocol with isolated mitochondria in a closed

respirometric chamber, defining a sequence of respiratory states.

547 548 Table 3. Metabolic states of mitochondria (Chance and Williams, 1956; Table V).

State	[ <b>O</b> <sub>2</sub> ]	ADP level	Substrate level	Respiration rate	Rate-limiting substance
1	>0	low	low	slow	ADP
2	>0	high	~0	slow	substrate
3	>0	high	high	fast	respiratory chain
4	>0	low	high	slow	ADP
5	0	high	high	0	oxygen

550

551 **State 1** is obtained after addition of isolated mitochondria to air-saturated 552 isoosmotic/isotonic respiration medium containing inorganic phosphate, but no fuel substrates 553 and no adenylates, *i.e.*, AMP, ADP, ATP.

554 State 2 is induced by addition of a high concentration of ADP (typically 100 to  $300 \,\mu$ M), 555 which stimulates respiration transiently on the basis of endogenous fuel substrates and 556 phosphorylates only a small portion of the added ADP. State 2 is then obtained at a low 557 respiratory activity limited by zero endogenous fuel substrate availability (**Table 3**). If addition 558 of specific inhibitors of respiratory complexes, such as rotenone, does not cause a further 559 decline of oxygen consumption, State 2 is equivalent to residual oxygen consumption (See 560 below). If inhibition is observed, undefined endogenous fuel substrates are a confounding factor 561 of pathway control by externally added substrates and inhibitors. In contrast to the original 562 protocol, an alternative sequence of titration steps is frequently applied, in which the alternative

State 2 has an entirely different meaning, when this second state is induced by addition of fuel
substrate without ADP (LEAK state; in contrast to State 3 as a ROX state as defined in Table
followed by addition of ADP.

566 State 3 is the state stimulated by addition of fuel substrates while the ADP concentration 567 is still high (Table 3) and supports coupled energy transformation through oxidative 568 phosphorylation. 'High ADP' is a concentration of ADP specifically selected to allow the 569 measurement of State 3 to State 4 transitions of isolated mitochondria in a closed respirometric 570 chamber. Repeated ADP titration re-establishes State 3 at 'high ADP'. Starting at oxygen 571 concentrations near air-saturation (ca. 200 µM O<sub>2</sub> at sea level and 37 °C), the total ADP 572 concentration added must be low enough (typically 100 to 300 µM) to allow phosphorylation 573 to ATP at a coupled oxygen consumption that does not lead to oxygen depletion during the 574 transition to State 4. In contrast, kinetically saturating ADP concentrations usually are an order 575 of magnitude higher than 'high ADP', e.g. 2.5 mM in isolated mitochondria. The abbreviation 576 State 3u is frequently used in bioenergetics, to indicate the state of respiration after titration of 577 an uncoupler, without sufficient emphasis on the fundamental difference between OXPHOS capacity (well-coupled with an endogenous uncoupled component) and ET capacity 578 579 (noncoupled).

580 State 4 is a LEAK state which is obtained only if the mitochondrial preparation is intact and well-coupled. Depletion of ADP by phosphorylation to ATP leads to a decline in oxygen 581 consumption in the transition from State 3 to State 4. Under these conditions, a maximum 582 protonmotive force and high ATP/ADP ratio are maintained, and the P»/O2 ratio can be 583 584 calculated. State 4 respiration,  $L_T$  (Table 1), reflects intrinsic proton leak and intrinsic ATP 585 hydrolysis activity. Oxygen consumption in State 4 is an overestimation of LEAK respiration 586 if the contaminating ATP hydrolysis activity recycles some ATP to ADP,  $J_{\text{eP}}$ , which stimulates respiration coupled to phosphorylation,  $J_{P} > 0$ . This can be tested by inhibition of the 587 588 phosphorylation pathway using oligomycin, ensuring that  $J_{P}=0$  (State 40). Alternatively, sequential ADP titrations re-establish State 3, followed by State 3 to State 4 transitions while
sufficient oxygen is available. However, anoxia may be reached before exhaustion of ADP
(State 5).

592 State 5 is the state after exhaustion of oxygen in a closed respirometric chamber. 593 Diffusion of oxygen from the surroundings into the aqueous solution may be a confounding 594 factor preventing complete anoxia (Gnaiger 2001). Chance and Williams (1955) provide an 595 alternative definition of State 5, which gives it the meaning of ROX: 'State 5 may be obtained 596 by antimycin A treatment or by anaerobiosis'.

In **Table 3**, only States 3 and 4 (and 'State 2' in the alternative protocol without ADP; not included in the table) are coupling control states, with the restriction that O<sub>2</sub> flux in State 3 may be limited kinetically by non-saturating ADP concentrations (**Table 1**).

600

#### 601 **3.** The protonmotive force and proton flux

## 602 3.1. Electric and chemical partial forces versus electrical and chemical units

The protonmotive force across the inner mitochondrial membrane (Mitchell and Moyle
1967) was introduced most beautifully in the *Grey Book 1966* (see Mitchell 2011),

605

$$\Delta p_{\rm H+} = \Delta \Psi + \Delta \mu_{\rm H+} / F \tag{Eq. 1}$$

The protonmotive force consists of two partial forces: (1) The electrical part,  $\Delta \Psi$ , is the difference of charge (electric potential difference) and is not specific for H<sup>+</sup>. (2) The chemical part,  $\Delta \mu_{H^+}$ , is the chemical potential difference in H<sup>+</sup>, is proportional to the pH difference, and incorporates the Faraday constant (**Table 4**).

- 610
- 611
- 612

613

**Table 4. Protonmotive force and flux matrix.** Rows: Electrical and chemical isomorphic format (*e* and *n*). The Faraday constant, *F*, converts protonmotive force and flux from *isomorphic format e* to *n*. Columns: The protonmotive force is the sum of *partial isomorphic forces*  $F_{el}$  and  $F_{H+,d}$ . In contrast to force (state), the conjugated flux

619 (rate) cannot be partitioned.620

State		Force		electric	+	chem.	Unit	Notes
	Protonmotive force, e	$\Delta p_{ m H^+}$	=	$\Delta \Psi$	+	$\Delta \mu_{ m H+}/F$	$J \cdot C^{-1}$	1 <i>e</i>
	Chemiosmotic potential, n	$\Delta \widetilde{\mu}_{{}_{H^{+}}}$	=	$\Delta \Psi \cdot F$	+	$\Delta \mu_{\mathrm{H}^+}$	$J \cdot mol^{-1}$	1 <i>n</i>
State	Isomorphic force	$F_{\mathrm{H}+,\mathrm{out}/i}$		elout	+	$\mathbf{H}^{+}_{\mathrm{out,d}}$		
	Electric charge, e	$F_{\mathrm{H}+,\mathrm{out}/e}$	=	$F_{\mathrm{el,out/}e}$	+	$F_{\mathrm{H}+,\mathrm{out,d}/e}$	J·C <sup>-1</sup>	2 <i>e</i>
	Amount of substance, <i>n</i>	$F_{\mathrm{H}+,\mathrm{out}/n}$	=	$F_{\mathrm{el,out}/n}$	+	$F_{\mathrm{H}+,\mathrm{out,d}/n}$	J·mol <sup>-1</sup>	2 <i>n</i>
Rate	Isomorphic flux	$J_{\mathrm{H}+,\mathrm{out}/i}$		e	or	n		
	Electric charge, e	$J_{\mathrm{H}+,\mathrm{out}/e}$		$J_{\mathrm{H}+,\mathrm{out}/e}$			$C \cdot s^{-1} \cdot m^{-3}$	3 <i>e</i>
	Amount of substance, n	$J_{\mathrm{H}+,\mathrm{out}/n}$				$J_{\mathrm{H}+,\mathrm{out}/n}$	$mol \cdot s^{-1} \cdot m^{-3}$	3 <i>n</i>

621

622 1: The Faraday constant, *F*, is the product of elementary charge ( $e=1.602177 \cdot 10^{-19}$ .C) and the 623 Avogadro (Loschmidt) constant ( $N_A=6.022136 \cdot 10^{23} \cdot \text{mol}^{-1}$ ),  $F=eN_A=96,485.3$  C/mol.  $\Delta \widetilde{\mu}_{H+}$  is the 624 chemiosmotic potential difference. 1*e* and 1*n* are the classical representations of 2*e* and 2*n*.

2: The protonmotive force is  $F_{H+,out}$ , expressed either in isomorphic format *e* or *n*.  $F_{el/e} \equiv \Delta \Psi$  is the partial protonmotive force (el) acting generally on charged motive molecules (*i.e.* ions that are displaceable across the inner mitochondrial membrane). In contrast,  $F_{H+,d/n} \equiv \Delta \mu_{H+}$  is the partial protonmotive force specific for proton displacement (H+d). The sign of the force is negative for exergonic transformations in which exergy is lost or dissipated, and positive for endergonic transformations which conserve exergy from a coupled exergonic process (**Box 3**).

3: The sign of the flux depends on the definition of the compartmental direction of the translocation (Fig.
2). Flux x force = J<sub>H+,out/e</sub>·F<sub>H+,out/e</sub> = J<sub>H+,out/n</sub>·F<sub>H+,out/n</sub> = Volume-specific power [J·s<sup>-1</sup>·m<sup>-3</sup>=W·m<sup>-3</sup>].

633

**Faraday constant**,  $F = eN_A$  [C/mol] (**Table 4**), enables the conversion between protonmotive force,  $F_{H+,out/e} \equiv \Delta p_{H+}$  [J/C], expressed per *motive charge*, *e* [C], and protonmotive force or electrochemical potential difference,  $F_{H+,out/n} \equiv \Delta \widetilde{\mu}_{H+} = \Delta p_{H+} \cdot F$  [J/mol], expressed per 637 *motive amount of protons*, n [mol]. Proton charge, e, and amount of substance, n, define the 638 units for the isomorphic formats. Taken together, F converts protonmotive force and flux from 639 isomorphic format e to n (Eq. 2; see also **Table 4**, Note 2),

- $F_{H+,out/n} = F_{H+,out/e} \cdot eN_A$  (Eq. 2.1)
- 641  $J_{H+,out/n} = J_{H+,out/e} / (eN_A)$  (Eq. 2.2)

In each format, the protonmotive force is expressed as the sum of two partial forces. The
concept expressed by the complex symbols in Eq. 1 can be explained and visualized more easily
by *partial isomorphic forces* as the components of the protonmotive force:

Electrical part of the protonmotive force: (1) Isomorph  $e: F_{el/e} \equiv \Delta \Psi$  is the electrical part of the protonmotive force expressed in units joule per coulomb, *i.e.* volt [V=J/C].  $F_{el/e}$  is defined as partial Gibbs energy change per *motive elementary charge*, e [C], not specific for proton charge (**Table 4**, Note 2e). (2) Isomorph  $n: F_{el/n} \equiv \Delta \Psi \cdot F$  is the electric force expressed in units joule per mole [J/mol], defined as partial Gibbs energy change per *motive amount of* charge, n [mol], not specific for proton charge (**Table 4**, Note 2n).

651 Chemical part of the protonmotive force: (1) Isomorph *n*:  $F_{d,H+/n} \equiv \Delta \mu_{H+}$  is the chemical 652 part (diffusion, displacement of H<sup>+</sup>) of the protonmotive force expressed in units joule per mole 653 [J/mol].  $F_{d,H+/n}$  is defined as partial Gibbs energy change per *motive amount of protons*, *n* [mol] 654 (**Table 4**, Note 2*n*). (2) Isomorph *e*:  $F_{d,H+/e} \equiv \Delta \mu_{H+}/F$  is the chemical force expressed in units 655 joule per coulomb [V], defined as partial Gibbs energy change per *motive amount of protons* 656 *expressed in units of electric charge, e* [C], but specific for proton charge (**Table 4**, Note 2*e*).

Protonmotive means that there is a potential for the movement of protons, and force is a measure of the potential for motion. Motion is relative and not absolute (Principle of Galilean Relativity); likewise there is no absolute potential, but (isomorphic) forces are potential differences. An electric partial force expressed in the format of electric charge,  $F_{el/e}$ , of -0.2 V (**Table 5**, Note 5*e*) is equivalent to force in the format of amount,  $F_{el,H+/n}$ , of 19 kJ·mol<sup>-1</sup> H<sup>+</sup><sub>out</sub> (Note 5*n*). For a ΔpH of 1 unit, the chemical partial force in the format of amount,  $F_{d,H+/n}$ , changes by 5.9 kJ·mol<sup>-1</sup> (**Table 5**, Note 6*n*) and chemical force in the format of charge  $F_{d,H+/e}$ changes by 0.06 V (Note 6*e*). Considering a driving force of -470 kJ·mol<sup>-1</sup> O<sub>2</sub> for oxidation, the thermodynamic limit of the H<sup>+</sup><sub>out</sub>/O<sub>2</sub> ratio is reached at a value of 470/19=24, compared to a mechanistic stoichiometry of 20 (**Fig. 1**).

667

668 *3.2. Definitions* 

669 Control and regulation: The terms metabolic *control* and *regulation* are frequently used synonymously, but are distinguished in metabolic control analysis: 'We could understand the 670 671 regulation as the mechanism that occurs when a system maintains some variable constant over 672 time, in spite of fluctuations in external conditions (homeostasis of the internal state). On the 673 other hand, metabolic control is the power to change the state of the metabolism in response to 674 an external signal' (Fell 1997). Respiratory control may be induced by experimental control 675 signals that *exert* an influence on: (1) ATP demand and ADP phosphorylation rate; (2) fuel 676 substrate composition, pathway competition; (3) available amounts of substrates and oxygen, 677 e.g., starvation and hypoxia; (3) the protonmotive force, redox states, flux-force relationships, coupling and efficiency; (4)  $Ca^{2+}$  and other ions including H<sup>+</sup>; (5) inhibitors, *e.g.*, nitric oxide 678 679 or intermediary metabolites, such as oxaloacetate; (6) signalling pathways and regulatory 680 proteins, e.g. insulin resistance, transcription factor HIF-1 or inhibitory factor 1. Mechanisms of respiratory control and regulation include adjustments of (1) enzyme activities by allosteric 681 682 mechanisms and phosphorylation, (2) enzyme content, concentrations of cofactors and 683 conserved moieties (such as adenylates, nicotinamide adenine dinucleotide [NAD<sup>+</sup>/NADH], coenzyme Q, cytochrome c); (3) metabolic channeling by supercomplexes; and (4) 684 685 mitochondrial density (enzyme concentrations and membrane area) and morphology (cristae 686 folding, fission and fusion). (5) Mitochondria are targeted directly by hormones, thereby 687 affecting their energy metabolism (Lee et al. 2013; Gerö and Szabo 2016; Price and Dai 2016; 688 Moreno et al. 2017). Evolutionary or acquired differences in the genetic and epigenetic basis of mitochondrial function (or dysfunction) between subjects and gene therapy; age; gender,
biological sex, and hormone concentrations; life style including exercise and nutrition; and
environmental issues including thermal, atmospheric, toxicological and pharmacological
factors, exert an influence on all control mechanisms listed above (for reviews, see Brown 1992;
Gnaiger 1993a, 2009; 2014; Paradies *et al.* 2014; Morrow *et al.* 2017).

694 **Respiratory control and response:** Lack of control by a metabolic pathway, *e.g.* 695 phosphorylation pathway, does mean that there will be no response to a variable activating it, 696 e.g. [ADP]. However, the reverse is not true as the absence of a response to [ADP] does not 697 exclude the phosphorylation pathway from having some degree of control. The degree of 698 control of a component of the OXPHOS pathway on an output variable, such as oxygen flux, 699 will in general be different from the degree of control on other outputs, such as phosphorylation 700 flux or proton leak flux (Box 2). As such, it is necessary to be specific as to which input and 701 output are under consideration (Fell 1997). Therefore, the term respiratory control is elaborated 702 in more detail in the following section.

703 Respiratory coupling control: Respiratory control refers to the ability of mitochondria 704 to adjust oxygen consumption in response to external control signals by engaging various 705 mechanisms of control and regulation. Respiratory control is monitored in a mitochondrial 706 preparation under conditions defined as respiratory states. When phosphorylation of ADP to 707 ATP is stimulated or depressed, an increase or decrease is observed in electron flux linked to 708 oxygen consumption in respiratory coupling states of intact mitochondria ('controlled states' in 709 the classical terminology of bioenergetics). Alternatively, coupling of electron transfer with 710 phosphorylation is disengaged by disruption of the integrity of the inner mitochondrial 711 membrane or by uncouplers, functioning like a clutch in a mechanical system. The 712 corresponding coupling control state is characterized by high levels of oxygen consumption 713 without control by phosphorylation ('uncontrolled state'). Energetic coupling is defined in **Box** 714 4. Loss of coupling by intrinsic uncoupling and decoupling, or pathological dyscoupling lowers the efficiency. Such generalized uncoupling is different from switching to mitochondrial pathways that involve fewer than three proton pumps ('coupling sites': Complexes CI, CIII and CIV), bypassing CI through multiple electron entries into the Q-junction (**Fig. 1**). A bypass of CIII and CIV is provided by alternative oxidases, which reduce oxygen without proton translocation. Reprogramming of mitochondrial pathways may be considered as a switch of gears (changing the stoichiometry) rather than uncoupling (loosening the stoichiometry).

Pathway control states are obtained in mitochondrial preparations by depletion of endogenous substrates and addition to the mitochondrial respiration medium of fuel substrates (CHNO) and specific inhibitors, activating selected mitochondrial pathways (Fig. 1). Coupling control states and pathway control states are complementary, since mitochondrial preparations depend on an exogenous supply of pathway-specific fuel substrates and oxygen (Gnaiger 2014).

726

# 727 Box 2: Metabolic fluxes and flows: vectorial and scalar

In mitochondrial electron transfer (**Fig. 1**), vectorial transmembrane proton flux is coupled through the proton pumps CI, CIII and CIV to the catabolic flux of scalar reactions, collectively measured as oxygen flux. In **Fig. 2**, the scalar catabolic reaction, k, of oxygen consumption,  $J_{02,k}$  [mol·s<sup>-1</sup>·m<sup>-3</sup>], is expressed as oxygen flux per volume, V [m<sup>3</sup>], of the instrumental chamber (the system).

Fluxes are *vectors*, if they have *spatial* direction in addition to magnitude. A vector flux (surface-density of flow) is expressed per unit cross-sectional area,  $A [m^2]$ , perpendicular to the direction of flux. If *flows*, *I*, are defined as extensive quantities of the *system*, as vector or scalar flow, *I* or *I* [mol·s<sup>-1</sup>], respectively, then the corresponding vector and scalar *fluxes*, *J*, are obtained as  $J=I\cdot A^{-1}$  [mol·s<sup>-1</sup>·m<sup>-2</sup>] and  $J=I\cdot V^{-1}$  [mol·s<sup>-1</sup>·m<sup>-3</sup>], respectively, expressing flux as an area-specific vector or volume-specific scalar quantity.

739 Vectorial transmembrane proton flux,  $J_{H+,out}$ , is analyzed in a heterogenous 740 compartmental system as a quantity with *directional* but not *spatial* information. Translocation

of protons across the inner mitochondrial membrane has a defined direction, either from the 741 742 negative compartment (matrix space; N-phase) to the positive compartment (inter-membrane 743 space; P-phase) or vice versa (Fig. 2). The arrows defining the direction of the translocation 744 between the two compartments may point upwards or downwards, right or left, without any implication that these are actual directions in space. The 'upper' compartment of the P-phase is 745 746 neither above nor below the N-phase in a spatial sense, but can be visualized arbitrarily in a 747 figure as the upper compartment (Fig. 2). In general, the *compartmental direction* of vectorial translocation from the N-phase to the P-phase is defined by assigning the initial and final state 748 749 as ergodynamic compartments,  $H^+_{in} \rightarrow H^+_{out}$ , respectively, related to work (erg = work) that 750 must be performed to lift the proton from a lower to a higher electrochemical potential or from 751 the lower to the higher ergodynamic compartment (Gnaiger 1993b).

752 In direct analogy to *vectorial* translocation, the direction of a *scalar* chemical reaction, A 753  $\rightarrow$  B, is defined by assigning substrates and products, A and B, as ergodynamic compartments.  $O_2$  is defined as a substrate in respiratory  $O_2$  consumption, which together with the fuel 754 755 substrates comprises the substrate compartment of the catabolic reaction (Fig. 2). Volumespecific scalar  $O_2$  flux is coupled (**Box 4**) to vectorial translocation. In order to establish a 756 757 quantitative relation between the coupled fluxes, both  $J_{O2,k}$  and  $J_{H+,out}$  must be expressed in identical units ( $[mol \cdot s^{-1} \cdot m^{-3}]$  or  $[C \cdot s^{-1} \cdot m^{-3}]$ ), yielding the H<sup>+</sup>out/O<sub>2</sub> ratio (**Fig. 1**). The vectorial 758 759 proton flux in compartmental translocation has *compartmental direction*, distinguished from a 760 vector flux with spatial direction. Likewise, the corresponding protonmotive force is defined 761 as an electrochemical potential difference between two compartments, in contrast to a gradient 762 across the membrane or a vector force with defined spatial direction.

763

The steady-state: Mitochondria represent a thermodynamically open system functioning
 as a biochemical transformation system in non-equilibrium states. State variables (protonmotive
 force; redox states) and metabolic fluxes (*rates*) are measured in defined mitochondrial

respiratory states. Strictly, steady states can be obtained only in open systems, in which changes 767 768 due to *internal* transformations, *e.g.*, O<sub>2</sub> consumption, are instantaneously compensated for by 769 external fluxes e.g., O<sub>2</sub> supply, such that oxygen concentration does not change in the system 770 (Gnaiger 1993b). Mitochondrial respiratory states monitored in closed systems satisfy the 771 criteria of pseudo-steady states for limited periods of time, when changes in the system 772 (concentrations of  $O_2$ , fuel substrates, ADP,  $P_i$ ,  $H^+$ ) do not exert significant effects on metabolic 773 fluxes (respiration, phosphorylation). Such pseudo-steady states require respiratory media with 774 sufficient buffering capacity and kinetically saturating concentrations of substrates to be 775 maintained, and thus depend on the kinetics of the processes under investigation. Proton 776 turnover,  $J_{\infty H^+}$ , and ATP turnover,  $J_{\infty P}$ , proceed in the steady-state at constant  $F_{H^+,out}$ , when  $J_{\infty H^+}$ 777  $= J_{H+,out} = J_{H+,in}$ , and at constant  $F_{P*}$ , when  $J_{\infty P} = J_{P*} = J_{\otimes P}$  (Fig. 2).

778

## 779 Box 3: Endergonic and exergonic transformations, exergy and dissipation

A chemical reaction, or any transformation, is exergonic if the Gibbs energy change (exergy) of the reaction is negative at constant temperature and pressure. The sum of Gibbs energy changes of all internal transformations in a system can only be negative, *i.e.* exergy is irreversibly dissipated. Endergonic reactions are characterized by positive Gibbs energies of reaction and cannot proceed spontaneously in the forward direction as defined. For instance, the endergonic reaction P» is coupled to exergonic catabolic reactions, such that the total Gibbs energy change is negative, *i.e.* exergy must be dissipated for the reaction to proceed (**Fig. 2**).

In contrast, energy cannot be lost or produced in any internal process, which is the key message of the first law of thermodynamics. Thus mitochondria are the sites of energy transformation but not energy production. Open and closed systems can gain energy and exergy only by external fluxes, *i.e.* uptake from the environment. Exergy is the potential to perform work. In the framework of flux-force relationships (**Box 4**), the *partial* derivative of Gibbs energy per advancement of a transformation is an isomorphic force,  $F_{tr}$  (**Table 5**, Note 2). In other words, force is equal to exergy/motive unit (in integral form, this definition takes care of non-isothermal processes). This formal generalization represents an appreciation of the conceptual beauty of Peter Mitchell's innovation of the protonmotive force against the background of the established paradigm of the electromotive force (emf) defined at the limit of zero current (Cohen *et al.* 2008).

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- 800 801

802

# Table 5. Power, exergy, force, flux, and advancement.

Expression	Symbol	Definition	Unit	Notes
Power, volume-specific	$P_{V,tr}$	$P_{V,tr} = J_{tr} \cdot F_{tr} = \partial_{tr} G \cdot \partial f^{-1}$	W=J·s <sup>-1</sup> ·m <sup>-3</sup>	1
Force, isomorphic	$F_{ m tr}$	$F_{\rm tr} = \partial_{\rm tr} G \cdot \partial_{\rm tr} \zeta^{-1}$	$J \cdot x^{-1}$	2
Flux, isomorphic	$J_{ m tr}$	$J_{\rm tr} = {\rm d}_{\rm tr} \boldsymbol{\xi} \cdot {\rm d} t^{-1} \cdot V^{-1}$	$x \cdot s^{-1} \cdot m^{-3}$	3
Advancement, n	$d_{tr}\xi_{H+/n}$	$\mathbf{d}_{\mathrm{tr}}\xi_{\mathrm{H}+/n} = \mathbf{d}_{\mathrm{tr}}n_{\mathrm{H}+} \cdot v_{\mathrm{H}+}^{-1}$	Mol	4 <i>n</i>
Advancement, e	$d_{tr}\xi_{H+/e}$	$\mathbf{d}_{\mathrm{tr}}\boldsymbol{\zeta}_{\mathrm{H}+/e} = \mathbf{d}_{\mathrm{tr}}\boldsymbol{e}_{\mathrm{H}+}\boldsymbol{\cdot}\boldsymbol{v}_{\mathrm{H}+}^{-1}$	С	4 <i>e</i>
Electric partial force, e	$F_{\mathrm{el}/e}$	$F_{\mathrm{el}/e} \equiv \Delta \Psi$	V	5 <i>e</i>
Electric partial force, n	$F_{\mathrm{el}/n}$	$\Delta \Psi \cdot F = 96.5 \cdot \Delta \Psi$	kJ·mol⁻¹	5 <i>n</i>
Chemical partial force, e	$F_{\mathrm{d,H+/}e}$	$\Delta \mu_{\rm H+}/F = - \ln(10) \cdot RT/F \cdot \Delta p H$	V	6 <i>e</i>
at 37 °C		= -0.06·ΔpH	J·C <sup>-1</sup>	
Chemical partial force, <i>n</i> at 37 °C	$F_{\mathrm{d,H+}/n}$	$\Delta \mu_{\rm H+} = -\ln(10) \cdot RT \cdot \Delta p H$ $= -5.9 \cdot \Delta p H$	J∙mol <sup>-1</sup> kJ∙mol <sup>-1</sup>	6 <i>n</i>

1 to 4: An isomorphic motive entity or transformant, expressed in units x, is defined for any
transformation, tr. x=mol or C in proton translocation.

805 2:  $\partial_{tr}G[J]$  is the partial Gibbs energy change in the advancement of transformation tr.

806 3: For x=C, flow is electric current,  $I_{el}$  [A = C·s<sup>-1</sup>], vector flux is electric current density per area,  $J_{el}$ , 807 and compartmental flux is electric current density per volume,  $I_{el}$  [A·m<sup>-3</sup>].

808 4*n*: For a chemical reaction, the advancement of reaction r is  $d_r\xi_B = d_r n_B \cdot v_B^{-1}$  [mol]. The stoichiometric 809 number is  $v_B = -1$  or  $v_B = 1$ , depending on B being a product or substrate, respectively, in reaction r 810 involving one mole of B. The conjugated *intensive* molar quantity,  $F_{B,r} = \partial_r G/\partial_r\xi_B$  [J·mol<sup>-1</sup>], is the 811 chemical force of reaction or reaction-motive force per stoichiometric amount of B. In reaction 812 kinetics,  $d_r n_B$  is expressed as a volume-specific quantity, which is the partial contribution to the 813 total concentration change of B,  $d_r c_B = d_r n_B / V$  and  $dc_B = dn_B / V$ , respectively. In open systems with 814 constant volume V,  $dc_B = d_r c_B + d_e c_B$ , where r indicates the *internal* reaction and e indicates the 815 external flux of B into the unit volume of the system. At steady state the concentration does not 816 change,  $dc_B=0$ , when  $d_rc_B$  is compensated for by the external flux of B,  $d_rc_B=-d_ec_B$  (Gnaiger 817 1993b). Alternatively,  $dc_B=0$  when B is held constant by different coupled reactions in which B 818 acts as a substrate or a product.

819 4*e*: Scalar potential difference across the mitochondrial membrane. In a scalar electric transformation 820 (flux of charge, *i.e.* volume-specific current, from the matrix space to the intermembrane and 821 extramitochondrial space) the motive force is the difference of charge (**Box 2**). The endergonic 822 direction of translocation is defined in **Fig. 2** as  $H^{+}_{in} \rightarrow H^{+}_{out}$ .

823 5*n*: *F*=96.5 (kJ·mol<sup>-1</sup>)/V.

824 6: The electric partial force is independent of temperature (Note 5), but the chemical partial force
825 depends on absolute temperature, *T* [K].

826 6e: RT is the gas constant times absolute temperature.  $\ln(10) \cdot RT/F = 59.16$  and 61.54 mV at 298.15 827 and 310.15 K (25 and 37 °C), respectively.

828 6*n*:  $\ln(10) \cdot RT = 5.708$  and 5.938 kJ·mol<sup>-1</sup> at 298.15 and 310.15 K (25 and 37 °C), respectively.

829

# 830 *3.3.* Forces and fluxes in physics and irreversible thermodynamics

831 According to its definition in physics, a potential difference and as such the 832 protonmotive force,  $\Delta p_{H+}$ , is not a force per se (Cohen et al. 2008). The fundamental forces of physics are distinguished from *motive forces* of statistical and irreversible thermodynamics. 833 834 Complementary to the attempt towards unification of fundamental forces defined in physics, the concepts of Nobel laureates Lars Onsager, Erwin Schrödinger, Ilya Prigogine and Peter 835 Mitchell (even if expressed in apparently unrelated terms) unite the diversity of generalized or 836 'isomorphic' flux-force relationships, the product of which links to the dissipation function and 837 Second Law of thermodynamics (Schrödinger 1944; Prigogine 1967). A motive force is the 838 839 derivative of potentially available or 'free' energy (exergy) per isomorphic *motive* unit (Box 3). Perhaps the first account of a *motive force* in energy transformation can be traced back to the
Peripatetic school around 300 BC in the context of moving a lever, up to Newton's motive force
proportional to the alteration of motion (Coopersmith 2010).

Vectorial and scalar forces, and fluxes: In chemical reactions and osmotic or diffusion 843 844 processes occurring in a closed heterogeneous system, such as a chamber containing isolated 845 mitochondria, scalar transformations occur without measured spatial direction but between 846 separate compartments (translocation between the matrix and intermembrane space) or between 847 energetically-separated chemical substances (reactions from substrates to products). Hence, the 848 corresponding fluxes are not vectorial but scalar, and are expressed per volume and not per 849 membrane area (Box 2). The corresponding motive forces are also scalar potential *differences* 850 across the membrane (Table 5), without taking into account the *gradients* across the 6 nm thick 851 inner mitochondrial membrane (Rich 2003).

**Coupling:** In energetics (ergodynamics), coupling is defined as an exergy transformation fuelled by an exergonic (downhill) input process driving the advancement of an endergonic (uphill) output process. The (negative) output/input power ratio is the efficiency of a coupled energy transformation (**Box 4**). At the limit of maximum efficiency of a completely coupled system, the (negative) input power equals the (positive) output power, such that the total power approaches zero at the maximum efficiency of 1, and the process becomes fully reversible without any dissipation of exergy, *i.e.* without entropy production.

859

# 860 Box 4: Coupling, power and efficiency, at constant temperature and pressure

Energetic coupling means that two processes of energy transformation are linked such that the input power,  $P_{in}$ , is the driving element of the output power,  $P_{out}$ , and the out/input power ratio is the efficiency. In general, power is work per unit time [J.s<sup>-1</sup>=W]. When describing a system with volume *V* without information on the internal structure, the output is defined as the *external* work (exergy) performed by the *total* system on its environment. Such a system may be open

for any type of exchange, or closed and thus allowing only heat and work to be exchanged 866 867 across the system boundaries. This is the classical black box approach of thermodynamics. In 868 contrast, in a colourful compartmental analysis of *internal* energy transformations (Fig. 2), the 869 system is structured and described by definition of ergodynamic compartments (with 870 information on the heterogeneity of the system; Box 2) and analysis of separate parts, *i.e.* a sequence of *partial* energy transformations, tr. In general, power per unit volume,  $P_{tr}/V$  [W.L<sup>-1</sup>], 871 872 is the product of a volume-specific flux,  $J_{tr}$ , and its conjugated force,  $F_{tr}$ , and is closely linked to the dissipation function using the terminology of irreversible thermodynamics (Prigogine 873 874 1967; Gnaiger 1993a,b). Output power of proton translocation and catabolic input power are 875 (Fig. 2),

876 Output: 
$$P_{\text{H+,out}}/V = J_{\text{H+,out}} \cdot F_{\text{H+,out}}$$

877 Input:

878  $F_{O2,k}$  is the exergonic input force with a negative sign, and,  $F_{H+,out}$ , is the endergonic output 879 force with a positive sign (**Box 3**). Ergodynamic efficiency is the ratio of output/input power, 880 or the flux ratio times force ratio (Gnaiger 1993a,b),

 $P_k/V = J_{O2,k} \cdot F_{O2,k}$ 

881 
$$\varepsilon = \frac{P_{\text{H+,out}}}{-P_{\text{k}}} = \frac{J_{\text{H+,out}}}{J_{\text{O2,k}}} \cdot \frac{F_{\text{H+,out}}}{-F_{\text{O2,k}}}$$

882 The concept of incomplete coupling relates exclusively to the first term, *i.e.* the flux ratio, or 883 H<sup>+</sup><sub>out</sub>/O<sub>2</sub> ratio (**Fig. 1**). Likewise, respirometric definitions of the P»/O<sub>2</sub> ratio and biochemical coupling efficiency (Section 3.2) consider flux ratios. In a completely coupled process, the 884 power efficiency,  $\varepsilon$ , depends entirely on the force ratio, ranging from zero efficiency at an 885 output force of zero, to the limiting output force and maximum efficiency of 1.0, when the total 886 power of the coupled process,  $P_t=P_k+P_{H+,out}$ , equals zero, and any net flows are zero at 887 888 ergodynamic equilibrium of a coupled process. Thermodynamic equilibrium is defined as the state when all potentials (all forces) are dissipated and equilibrate towards their minima of zero. 889 890 In a fully or completely coupled process, output and input fluxes are directly proportional in a 894

Coupled versus bound processes: Since the chemiosmotic theory describes the 895 mechanisms of coupling in OXPHOS, it may be interesting to ask if the electrical and chemical 896 897 parts of proton translocation are coupled processes. This is not the case according to the 898 definition of coupling. If the coupling mechanism is disengaged, the output process becomes 899 independent of the input process, and both proceed in their downhill (exergonic) direction (Fig. 900 2). It is not possible to physically uncouple the electrical and chemical processes, which are 901 only theoretically partitioned as electrical and chemical components and can be measured 902 separately. If partial processes are non-separable, *i.e.*, cannot be uncoupled, then these are not 903 coupled but are defined as bound processes. The electrical and chemical parts are tightly bound 904 partial forces of the protonmotive force, since a flux cannot be partitioned but expressed only 905 in either an electrical or chemical isomorphic format (Table 4).

906

907 **4. Normalization: fluxes and flows** 

The challenges of measuring mitochondrial respiratory flux are matched by those of normalization, whereby  $O_2$  consumption may be considered as the nominator and normalization as the complementary denominator, which are tightly linked in reporting the measurements in a format commensurate with the requirements of a database.

912

# 913 *4.1. Flux per chamber volume*

914 When the reactor volume does not change during the reaction, which is typical for liquid 915 phase reactions, the volume-specific *flux of a chemical reaction* r is the time derivative of the 916 advancement of the reaction per unit volume,  $J_{V,B} = d_r \zeta_B / dt \cdot V^{-1}$  [(mol·s<sup>-1</sup>)·L<sup>-1</sup>]. The *rate of* 

concentration change is  $dc_B/dt$  [(mol·L<sup>-1</sup>)·s<sup>-1</sup>], where concentration is  $c_B=n_B/V$ . It is helpful to 917 make the subtle distinction between  $[mol \cdot s^{-1} \cdot L^{-1}]$  and  $[mol \cdot L^{-1} \cdot s^{-1}]$  for the fundamentally 918 different quantities of volume-specific flux and rate of concentration change, which merge to a 919 920 single expression only in closed systems. In open systems, external fluxes (such as O<sub>2</sub> supply) 921 are distinguished from internal transformations (metabolic flux, O<sub>2</sub> consumption). In a closed 922 system, external flows of all substances are zero and  $O_2$  consumption (internal flow),  $I_{O2}$ 923 [pmol·s<sup>-1</sup>], causes a decline of the amount of O<sub>2</sub> in the system,  $n_{O2}$  [nmol]. Normalization of these quantities for the volume of the system, V [L= $dm^3$ ], yields volume-specific O<sub>2</sub> flux, 924  $J_{V,O2}=I_{O2}/V$  [nmol·s<sup>-1</sup>·L<sup>-1</sup>], and O<sub>2</sub> concentration, [O<sub>2</sub>] or  $c_{O2}=n_{O2}/V$  [nmol·mL<sup>-1</sup>=µmol·L<sup>-1</sup>=µM]. 925 926 Instrumental background O<sub>2</sub> flux is due to external flux into a non-ideal closed respirometer, such that total volume-specific flux has to be corrected for instrumental background O<sub>2</sub> flux, 927 *i.e.*  $O_2$  diffusion into or out of the instrumental chamber.  $J_{V,O2}$  is relevant mainly for 928 929 methodological reasons and should be compared with the accuracy of instrumental resolution of background-corrected flux, e.g. ±1 nmol·s<sup>-1</sup>·L<sup>-1</sup> (Gnaiger 2001). 'Metabolic' or catabolic 930 931 indicates O<sub>2</sub> flux, J<sub>O2,k</sub>, corrected for instrumental background O<sub>2</sub> flux and chemical background O<sub>2</sub> flux due to autoxidation of chemical components added to the incubation medium. 932

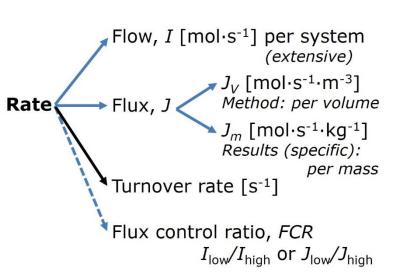
933

### 934 *4.2. System-specific and sample-specific normalization*

Application of common and generally defined units is required for direct transfer of reported results into a database. The second [s] is the *SI* unit for the base quantity *time*. It is also the standard time-unit used in solution chemical kinetics. **Table 6** lists some conversion factors to obtain *SI* units. The term *rate* is not sufficiently defined to be useful for a database (**Fig. 7**). The inconsistency of the meanings of rate becomes fully apparent when considering Galileo Galilei's famous principle, that 'bodies of different weight all fall at the same rate (have a constant acceleration)' (Coopersmith 2010). 942 Extensive quantities: An extensive quantity increases proportionally with system size.
943 The magnitude of an extensive quantity is completely additive for non-interacting subsystems,
944 such as mass or flow expressed per defined system. The magnitude of these quantities depends
945 on the extent or size of the system (Cohen *et al.* 2008).

946

947 Fig. 7. Different meanings of rate may lead to confusion, if the 948 949 normalization is not sufficiently 950 specified. Results are frequently 951 expressed as mass-specific flux, Jm, 952 per mg protein, dry or wet weight 953 (mass). Cell volume, V<sub>cell</sub>, or 954 mitochondrial volume, Vmt, may be 955 used for normalization (volume-



956 specific flux,  $J_{Vcell}$  or  $J_{Vmt}$ ), which then must be clearly distinguished from flux,  $J_V$ , expressed for 957 methodological reasons per volume of the measurement system, or flow per cell,  $I_X$ .

958

**Size-specific quantities:** 'The adjective *specific* before the name of an extensive quantity is often used to mean *divided by mass*' (Cohen *et al.* 2008). Mass-specific flux is flow divided by mass of the system. A mass-specific quantity is independent of the extent of non-interacting homogenous subsystems. Tissue-specific quantities are of fundamental interest in comparative mitochondrial physiology, where *specific* refers to the *type* rather than *mass* of the tissue. The term *specific*, therefore, must be further clarified, such that tissue mass-specific, *e.g.*, muscle mass-specific quantities are defined.

Molar quantities: 'The adjective *molar* before the name of an extensive quantity generally means *divided by amount of substance*' (Cohen *et al.* 2008). The notion that all molar quantities then become *intensive* causes ambiguity in the meaning of *molar Gibbs energy*. It is important to emphasize the fundamental difference between normalization for amount of substance *in a system* or for amount of motive substance *in a transformation*. When the Gibbs energy of a system, *G* [J], is divided by the amount of substance B in the system,  $n_B$  [mol], a *size-specific* molar quantity is obtained,  $G_B = G/n_B$  [J·mol<sup>-1</sup>], which is not any force at all. In contrast, when the partial Gibbs energy change,  $\partial_r G$  [J], is divided by the motive amount of substance B in reaction r (advancement of reaction),  $\partial_r \zeta_B$  [mol], the resulting intensive molar quantity,  $F_{r,B} = \partial G/\partial_r \zeta_B$  [J·mol<sup>-1</sup>], is the chemical motive force of reaction r involving 1 mol B (**Table 5**, Note 4).

Flow per system, *I*: In analogy to electrical terms, flow as an extensive quantity (*I*; per system) is distinguished from flux as a size-specific quantity (*J*; per system size) (Fig. 7). Electric current is flow,  $I_{el}$  [A=C·s<sup>-1</sup>] per system (extensive quantity). When dividing this extensive quantity by system size (membrane area), a size-specific quantity is obtained, which is electric flux (electric current density),  $J_{el}$  [A·m<sup>-2</sup> = C·s<sup>-1</sup>·m<sup>-2</sup>].

982 Size-specific flux, J: Metabolic O<sub>2</sub> flow per tissue increases as tissue mass is increased. 983 Tissue mass-specific O<sub>2</sub> flux should be independent of the size of the tissue sample studied in 984 the instrument chamber, but volume-specific O<sub>2</sub> flux (per volume of the instrument chamber, V) should increase in direct proportion to the amount of sample in the chamber. Accurate 985 986 definition of the experimental system is decisive: whether the experimental chamber is the 987 closed, open, isothermal or non-isothermal system with defined volume as part of the 988 measurement apparatus, in contrast to the experimental *sample* in the chamber (**Table 6**). 989 Volume-specific  $O_2$  flux depends on mass-concentration of the sample in the chamber, but 990 should be independent of the chamber volume. There are practical limitations to increasing the 991 mass-concentration of the sample in the chamber, when one is concerned about crowding 992 effects and instrumental time resolution.

993 Sample concentration  $C_{mX}$ : Normalization for sample concentration is required for 994 reporting respiratory data. Consider a tissue or cells as the sample, *X*, and the sample mass,  $m_X$ 995 [mg] from which a mitochondrial preparation is obtained. The sample mass is frequently

measured as wet or dry weight ( $m_X \equiv W_w$  or  $W_d$  [mg]), or as amount of tissue or cell protein 996 997  $(m_X \equiv m_{\text{Protein}})$ . In the case of permeabilized tissues, cells, and homogenates, the sample concentration,  $C_{mX}=m_X/V$  [mg·mL<sup>-1</sup>=g·L<sup>-1</sup>], is simply the mass of the subsample of tissue that is 998 transferred into the instrument chamber. Part of the mitochondria from the tissue is lost during 999 1000 preparation of isolated mitochondria, and only a fraction of mitochondria is obtained, expressed as the mitochondrial yield (Fig. 8). At a high mitochondrial yield the sample of isolated 1001 1002 mitochondria is more representative of the total mitochondrial population than in preparations 1003 characterized by low mitochondrial yield. Determination of the mitochondrial yield is based on 1004 measurement of the concentration of a mitochondrial marker in the tissue homogenate,  $C_{\rm mte,thom}$ , 1005 which simultaneously provides information on the specific mitochondrial density in the sample 1006 (**Fig. 8**).

Tissues can contain multiple cell populations which may have distinct mitochondrial 1007 1008 subtypes. Mitochondria are also in a constant state of flux due to highly dynamic fission and 1009 fusion cycles, and can exist in multiple stages and sizes which may be altered by a range of factors. The isolation of mitochondria (often achieved through differential centrifugation) can 1010 1011 therefore yield a subsample of the mitochondrial types present in a tissue, dependent on 1012 isolation protocols utilized (e.g. centrifugation speed). This possible artefact should be taken 1013 into account when planning experiments using isolated mitochondria. The tendency for 1014 mitochondria of specific sizes to be enriched at different centrifugation speeds also has the potential to allow the isolation of specific mitochondrial subpopulations and therefore the 1015 1016 analysis of mitochondria from multiple cell lineages within a single tissue.

1017 **Mass-specific flux**,  $J_{mX,02}$ : Mass-specific flux is obtained by expressing respiration per 1018 mass of sample,  $m_X$  [mg]. X is the type of sample, e.g., tissue homogenate, permeabilized fibres 1019 or cells. Volume-specific flux is divided by mass concentration of X,  $J_{mX,02} = J_{V,02}/C_{mX}$ ; or flow 1020 per cell is divided by mass per cell,  $J_{mcell,02} = I_{cell,02}/M_{cell}$ . If mass-specific O<sub>2</sub> flux is constant 1021 and independent of sample size (expressed as mass), then there is no interaction between the subsystems. A 1.5 mg and a 3.0 mg muscle sample respires at identical mass-specific flux.
Mass-specific O<sub>2</sub> flux, however, may change with the mass of a tissue sample, cells or isolated
mitochondria in the measuring chamber, in which case the nature of the interaction becomes an
issue. Optimization of cell density and arrangement is generally important and particularly in
experiments carried out in wells, considering the confluency of the cell monolayer or clumps
of cells (Salabei *et al.* 2014).

1028

Expression	Symbol	Definition	SI Unit	Notes
Sample				
Identity of sample	X	Cells, animals, patients		
Number of sample entities X	$N_X$	Number of cells, etc.	Х	
Mass of sample <i>X</i>	$m_X$		kg	1
Mass of entity X	$M_X$	$M_X = m_X \cdot N_X^{-1}$	kg·x <sup>-1</sup>	1
Mitochondria				
Mitochondria	mt	X=mt		
Amount of mt-elements	mte	Quantity of mt-marker	X <sub>mte</sub>	
Concentrations				
Sample number concentration	$C_{NX}$	$C_{NX} = N_X \cdot V^{-1}$	x·m <sup>-3</sup>	2
Sample mass concentration	$C_{mX}$	$C_{mX} = m_X \cdot V^{-1}$	kg⋅m <sup>-3</sup>	
Mitochondrial concentration	$C_{\rm mte}$	$C_{\rm mte} = { m mte} \cdot V^{-1}$	$x_{mte} \cdot m^{-3}$	3
Specific mitochondrial density	$D_{\rm mte}$	$D_{\rm mte} = {\rm mte} \cdot m_X^{-1}$	x <sub>mte</sub> ·kg <sup>-1</sup>	4
Mitochondrial content, mte per entity X	mte <sub>X</sub>	$mte_X = mte \cdot N_X^{-1}$	$x_{mte} \cdot x^{-1}$	5
O <sub>2</sub> flow and flux				6
Flow	$I_{O2}$	Internal flow	mol·s <sup>-1</sup>	7
Volume-specific flux	$J_{V,O2}$	$J_{V,O2} = I_{O2} \cdot V^{-1}$	mol·s <sup>-1</sup> ·m <sup>-3</sup>	8
Flow per sample entity X	$I_{X,O2}$	$I_{X,O2} = J_{V,O2} \cdot C_{NX}^{-1}$	mol·s <sup>-1</sup> ·x <sup>-1</sup>	9
Mass-specific flux	$J_{mX,O2}$	$J_{mX,O2} = J_{V,O2} \cdot C_{mX}^{-1}$	mol·s <sup>-1</sup> ·kg <sup>-1</sup>	
Mitochondria-specific flux	$J_{\rm mte,O2}$	$J_{\rm mte,O2} = J_{V,O2} \cdot C_{\rm mte}^{-1}$	$mol \cdot s^{-1} \cdot x_{mte}^{-1}$	10

# 1029<br/>1030Table 6. Sample concentrations and normalization of flux with SI base units.

1031

1032 1 The SI prefix k is used for the SI base unit of mass (kg=1,000 g). In praxis, various SI prefixes are

used for convenience, to make numbers easily readable, *e.g.* 1 mg tissue, cell or mitochondrial massinstead of 0.000001 kg.

1035 2 In case X=cells, the sample number concentration is  $C_{\text{Ncell}}=N_{\text{cell}}\cdot V^1$ , and volume may be expressed

1036 in  $[dm^3=L]$  or  $[cm^3=mL]$ . See **Table 7** for different sample types.

1038 (2)  $C_{mte}=mte_X C_{NX}$ ; (3)  $C_{mte}=C_{mX} D_{mte}$ .

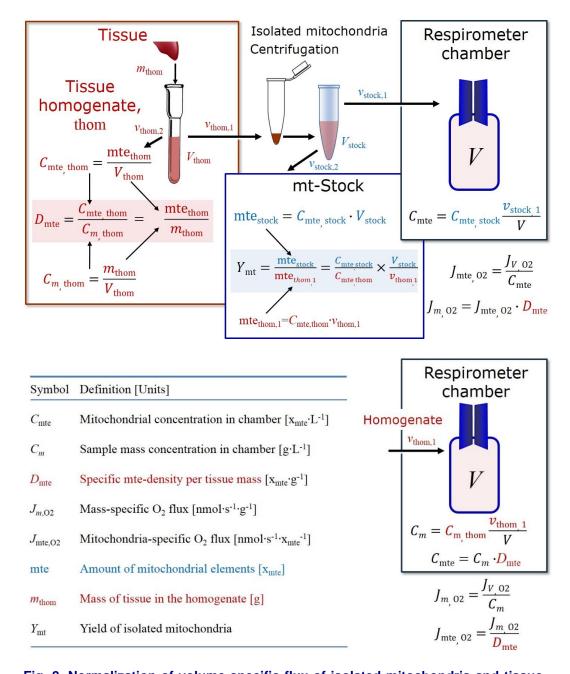
- 1039 4 If the amount of mitochondria, mte, is expressed as mitochondrial mass, then  $D_{mte}$  is the mass 1040 fraction of mitochondria in the sample. If mte is expressed as mitochondrial volume,  $V_{mt}$ , and the 1041 mass of sample,  $m_X$ , is replaced by volume of sample,  $V_X$ , then  $D_{mte}$  is the volume fraction of 1042 mitochondria in the sample.
- 1043 5 mte<sub>X</sub>=mte· $N_X^{-1}=C_{mte}\cdot C_{NX}^{-1}$ .
- 1044 6 Entity O<sub>2</sub> can be replaced by other chemical entities B to study different reactions.

10457 $l_{02}$  and V are defined per instrument chamber as a system of constant volume (and constant1046temperature), which may be closed or open.  $l_{02}$  is abbreviated for  $l_{02,r}$ , *i.e.* the metabolic or internal1047 $O_2$  flow of the chemical reaction r in which  $O_2$  is consumed, hence the negative stoichiometric1048number,  $v_{02}$ =-1.  $l_{02,r}$ =d<sub>r</sub> $n_{02}/dt$ · $v_{02}$ -1. If r includes all chemical reactions in which  $O_2$  participates, then1049d<sub>r</sub> $n_{02}$  = d $n_{02}$  - d<sub>e</sub> $n_{02}$ , where d $n_{02}$  is the change in the amount of  $O_2$  in the instrument chamber and1050d<sub>e</sub> $n_{02}$  is the amount of  $O_2$  added externally to the system. At steady state, by definition d $n_{02}$ =0, hence1051d<sub>r</sub> $n_{02}$ =-d<sub>e</sub> $n_{02}$ .

- 1052 8  $J_{V,O2}$  is an experimental variable, expressed per volume of the instrument chamber.
- 1053 9  $I_{X,O2}$  is a physiological variable, depending on the size of entity X.
- 1054 10 There are many ways to normalize for a mitochondrial marker, that are used in different experimental

1055 approaches: (1)  $J_{\text{mte},O2} = J_{V,O2} \cdot C_{\text{mte}^{-1}}$ ; (2)  $J_{\text{mte},O2} = J_{V,O2} \cdot C_{mX^{-1}} \cdot D_{\text{mte}^{-1}} = J_{mX,O2} \cdot D_{\text{mte}^{-1}}$ ; (3)  $J_{\text{mte},O2} = J_{02} \cdot C_{NX^{-1}} \cdot C_{NX^$ 

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- 1060
- 1061



1064Fig. 8. Normalization of volume-specific flux of isolated mitochondria and tissue1065homogenate. A: Mitochondrial yield, Ymt, in preparation of isolated mitochondria. zthom,11066and zstock,1 are the volumes transferred from the total volume, Vthom and Vstock, respectively.1067mtethom,1 is the amount of mitochondrial elements in volume zthom,1 used for isolation. B:1068In respirometry with homogenate, zthom,1 is transferred directly into the respirometer1069chamber. See Table 6 for further explanation of symbols.

1073	Table 7. Some useful abbreviations
1074	of various sample types, X.

Identity of sample	X
Mitochondrial preparations	mtprep
Isolated mitochondria	imt
Tissue homogenate	thom
Permeabilized tissue	pti
Permeabilized fibres	pfi
Permeabilized cells	pce
Cells	ce

1075

1076 **Number concentration**,  $C_{NX}$ : The experimental *number concentration* of sample in the 1077 case of cells or animals, *e.g.*, nematodes is  $C_{NX}=N_X/V$  [x·mL<sup>-1</sup>], where  $N_X$  is the number of cells 1078 or organisms in the chamber (**Table 6**).

1079 Flow per sample entity,  $I_{X,O2}$ : A special case of normalization is encountered in 1080 respiratory studies with permeabilized (or intact) cells. If respiration is expressed per cell, the 1081  $O_2$  flow per measurement system is replaced by the  $O_2$  flow per cell,  $I_{cell,O2}$  (Table 6).  $O_2$  flow can be calculated from volume-specific O<sub>2</sub> flux,  $J_{V,O2}$  [nmol·s<sup>-1</sup>·L<sup>-1</sup>] (per V of the measurement 1082 chamber [L]), divided by the number concentration of cells,  $C_{Nce} = N_{ce}/V$  [cell·L<sup>-1</sup>], where  $N_{ce}$  is 1083 the number of cells in the chamber. Cellular O<sub>2</sub> flow can be compared between cells of identical 1084 1085 size. To take into account changes and differences in cell size, further normalization is required 1086 to obtain cell size-specific or mitochondrial marker-specific O<sub>2</sub> flux (Renner et al. 2003).

1087 The complexity changes when the sample is a whole organism studied as an experimental 1088 model. The well-established scaling law in respiratory physiology reveals a strong interaction 1089 of O<sub>2</sub> consumption and individual body mass of an organism, since *basal* metabolic rate (flow) 1090 does not increase linearly with body mass, whereas *maximum* mass-specific O<sub>2</sub> flux,  $\dot{V}_{O2max}$  or 1091  $\dot{V}_{O2peak}$ , is approximately constant across a large range of individual body mass (Weibel and 1092 Hoppeler 2005), with individuals, breeds, and certain species deviating substantially from this 1093 general relationship.  $\dot{V}_{02\text{peak}}$  of human endurance athletes is 60 to 80 mL O<sub>2</sub>·min<sup>-1</sup>·kg<sup>-1</sup> body 1094 mass, converted to  $J_{m,02\text{peak}}$  of 45 to 60 nmol·s<sup>-1</sup>·g<sup>-1</sup> (Gnaiger 2014; **Table 8**).

1095

### 1096 *4.3. Normalization for mitochondrial content*

1097 Normalization is a problematic subject and it is essential to consider the question of the study. If the study aims to compare tissue performance, such as the effects of a certain treatment 1098 1099 on a specific tissue, then normalization can be successful, using tissue mass or protein content, 1100 for example. If the aim, however, is to find differences of mitochondrial function independent 1101 of mitochondrial density (Table 6), then normalization to a mitochondrial marker is imperative. However, one cannot assume that quantitative changes in various markers such as 1102 1103 mitochondrial proteins necessarily occur in parallel with one another. It is important to first establish that the marker chosen is not selectively altered by the performed treatment. In 1104 1105 conclusion, the normalization must reflect the question under investigation to reach a satisfying 1106 answer. On the other hand, the goal of comparing results across projects and institutions requires some standardization on normalization for entry into a databank. 1107

1108 Mitochondrial concentration,  $C_{mte}$ , and mitochondrial markers: It is important that 1109 mitochondrial content in the tissue and the measurement chamber be quantified, as a physiological output and result of mitochondrial biogenesis and degradation, and as a quantity 1110 1111 for normalization in functional analyses. Mitochondrial organelles comprise a cellular reticulum that is in a continual flux of fusion and fission. Hence the definition of an "amount" 1112 of mitochondria is often misconceived: mitochondria cannot be counted as a number of 1113 occurring elements. Therefore, quantification of the "amount" of mitochondria depends on 1114 1115 measurement of chosen mitochondrial markers. 'Mitochondria are the structural and functional elemental units of cell respiration' (Gnaiger 2014). The quantity of a mitochondrial marker can 1116 1117 be considered as the measurement of the amount of *elemental mitochondrial units* or mitochondrial elements, mte. However, since mitochondrial quality changes under certain 1118

stimuli, particularly in mitochondrial dysfunction, some markers can vary while other markers 1119 1120 are unchanged. (1) Mitochondrial volume or membrane area are structural markers, whereas mitochondrial protein mass is frequently used as a marker for isolated 1121 mitochondria. (2)Molecular and enzymatic mitochondrial markers (amounts or activities) can be selected as 1122 1123 matrix markers, e.g., citrate synthase activity, mtDNA; or inner mt-membrane markers, e.g., cytochrome c oxidase activity,  $aa_3$  content, cardiolipin, TOM20. (3) Extending the 1124 1125 measurement of mitochondrial marker enzyme activity to mitochondrial pathway capacity, measured as ET or OXPHOS capacity, can be considered as an integrative functional 1126 1127 mitochondrial marker.

1128 Depending on the type of mitochondrial marker, the mitochondrial elements, mte, are 1129 expressed in marker-specific units. Although concentration and density are used synonymously 1130 in physical chemistry, it is recommended to distinguish *experimental mitochondrial* 1131 *concentration*,  $C_{mte}=mte/V$  and *physiological mitochondrial density*,  $D_{mte}=mte/m_X$ . Then 1132 mitochondrial density is the amount of mitochondrial elements per mass of tissue. The former 1133 is mitochondrial density multiplied by sample mass concentration,  $C_{mte}=D_{mte} \cdot C_{mX}$ , or 1134 mitochondrial content multiplied by sample number concentration,  $C_{mte}=mte_X \cdot C_{NX}$  (**Table 6**).

1135 Mitochondria-specific flux, J<sub>mte,O2</sub>: Volume-specific metabolic O<sub>2</sub> flux depends on: (1) 1136 the sample concentration in the volume of the instrument chamber,  $C_{mX}$ , or  $C_{NX}$ ; (2) the 1137 mitochondrial density in the sample,  $D_{\text{mte}}=\text{mte}/m_X$  or  $\text{mte}_X=\text{mte}/N_X$ ; and (3) the specific mitochondrial activity or performance per elemental mitochondrial unit,  $J_{\text{mte,O2}}=J_{V,O2}/C_{\text{mte}}$ 1138 1139 (Table 6). Obviously, the numerical results for  $J_{\rm mte,O2}$  vary according to the type of mitochondrial marker chosen for measurement of mte and  $C_{mte}=mte/V$ . Some problems are 1140 1141 common for all mitochondrial markers: (1) Accuracy of measurement is crucial, since even a highly accurate and reproducible measurement of O<sub>2</sub> flux becomes inaccurate and noisy if 1142 normalized for a biased and noisy measurement of a mitochondrial marker. This problem is 1143 1144 acute in mitochondrial respiration because the denominators used (the mitochondrial markers)

are often very small moieties whose accurate and precise determination is difficult. This 1145 1146 problem can be avoided when O<sub>2</sub> fluxes measured in substrate-uncoupler-inhibitor titration 1147 protocols are normalized for flux in a defined respiratory reference state, which is used as an internal marker and yields flux control ratios, FCRs (Fig. 7). FCRs are independent of any 1148 1149 externally measured markers and, therefore, are statistically very robust. FCRs indicate qualitative changes of mitochondrial respiratory control, with highest quantitative resolution, 1150 1151 separating the effect of mitochondrial density or concentration on  $J_{mX,O2}$  or  $I_{X,O2}$  from that of 1152 function per elemental mitochondrial marker,  $J_{mte,O2}$  (Pesta *et al.* 2011; Gnaiger 2014). (2) If 1153 mitochondrial quality does not change and only the amount of mitochondria, defined by the 1154 chosen mitochondrial marker, varies as a determinant of mass-specific flux, then any marker is 1155 equally qualified in principle; then in practice selection of the optimum marker depends only on the accuracy and precision of measurement of the mitochondrial marker. (3) If mitochondrial 1156 1157 flux control ratios change, then there may not be any best mitochondrial marker. In general, measurement of multiple mitochondrial markers enables a comparison and evaluation of 1158 normalization for a variety of mitochondrial markers. 1159

1160

### 1161 *4.4. Evaluation of mitochondrial markers*

1162 Different methods are implicated in quantification of mitochondrial markers and have 1163 different strengths. Evaluation of mitochondrial markers in healthy controls is insufficient for providing guidelines for application in the diagnosis of pathological states and specific 1164 1165 treatments. In line with the concept of the respiratory control ratio (Chance and Williams 1955a), the most readily used normalization is that of flux control ratios and flux control factors 1166 1167 (Gnaiger 2014). Selection of the state of maximum flux in a protocol as the reference state has the advantages of (1) internal normalization, (2) statistical linearization of the response in the 1168 1169 range of 0 to 1, and (3) consideration of maximum flux for integrating a very large number of elemental steps in the OXPHOS or ET-pathways. This reduces the risk of selecting a functional 1170

marker that is specifically altered by the treatment or pathodology, yet increases the chance that 1171 1172 the highly integrative state is actually affected when compared with the controls. In this case, 1173 additional information can be obtained by reporting flux control ratios based on a reference 1174 state which indicates stable tissue-mass specific flux, *e.g.* the OXPHOS rather than ET state. 1175 Stereological determination of mitochondrial content via two-dimensional transmission 1176 electron microscopy can have limitations due to the dynamics of mitochondrial size (Meinild 1177 Lundby et al. 2017). Accurate determination of three-dimensional volume by two-dimensional 1178 microscopy can be both time consuming and statistically challenging (Larsen *et al.* 2012). 1179 Using mitochondrial marker enzymes (citrate synthase activity, Complex I-IV amount or 1180 activity) for normalization of flux is limited in part by the same factors that apply to the use of 1181 flux control ratios. Strong correlations between various mitochondrial markers and citrate synthase activity [1, 11, 12] are expected in a specific tissue of healthy subjects. Citrate synthase 1182 1183 activity has been shown to be acutely modifiable by exercise [13, 14]. Evaluation of 1184 mitochondrial markers related to a selected age and sex cohort cannot be extrapolated to provide recommendations for normalization in respirometric diagnosis of disease, in different states of 1185 development and ageing, different cell types, tissues, and species. mtDNA normalised to nDNA 1186 1187 via qPCR is correlated to functional mitochondrial markers including OXPHOS and ET 1188 capacity in some cases (Boushel *et al.* 2007; [5-7]), lack of such correlations have been reported 1189 [2, 8, 9]. Several studies indicate a strong correlation between cardiolipin content and increase in mitochondrial functionality with exercise [1-4], but its use as a general mitochondrial 1190 1191 biomarker in disease remains questionable.

1192

### 1193 *4.5. Conversion: units and normalization*

1194 Many different units have been used to report the rate of oxygen consumption, OCR 1195 (**Table 8**). *SI* base units provide the common reference for introducing the theoretical principles 1196 (**Fig. 7**), and are used with appropriately chosen *SI* prefixes to express numerical data in the

most practical format, with an effort towards unification within specific areas of application 1197 1198 (**Table 9**). For studies of cells, we recommend that respiration be expressed, as far as possible, as (1) O<sub>2</sub> flux normalized for a mitochondrial marker, for separation of the effects of 1199 mitochondrial quality and content on cell respiration (this includes FCRs as a normalization for 1200 1201 a functional mitochondrial marker); (2)  $O_2$  flux in units of cell volume or mass, for comparison 1202 of respiration of cells with different cell size (Renner et al. 2003) and with studies on tissue preparations, and (3)  $O_2$  flow in units of attomole (10<sup>-18</sup> mol) of  $O_2$  consumed by each cell in a 1203 second [amol·s<sup>-1</sup>·cell<sup>-1</sup>], numerically equivalent to [pmol·s<sup>-1</sup>·10<sup>-6</sup> cells]. This convention allows 1204 1205 information to be easily used when designing experiments in which oxygen consumption must 1206 be considered. For example, to estimate the volume-specific O<sub>2</sub> flux in an instrument chamber that would be expected at a particular cell number concentration, one simply needs to multiply 1207 the flow per cell by the number of cells per volume of interest. This provides the amount of O<sub>2</sub> 1208 [mol] consumed per time [s<sup>-1</sup>] per unit volume [L<sup>-1</sup>]. At an O<sub>2</sub> flow of 100 amol·s<sup>-1</sup>·cell<sup>-1</sup> and a 1209 cell density of  $10^9$  cells·L<sup>-1</sup> ( $10^6$  cells·mL<sup>-1</sup>), the volume-specific O<sub>2</sub> flux is 100 nmol·s<sup>-1</sup>·L<sup>-1</sup> (100 1210 pmol·s<sup>-1</sup>·mL<sup>-1</sup>). 1211

Although volume is expressed as  $m^3$  using the SI base unit, the litre [dm<sup>3</sup>] is the basic unit 1212 of volume for concentration and is used for most solution chemical kinetics. If one multiplies 1213  $I_{cell,O2}$  by  $C_{Ncell}$ , then the result will not only be the amount of O<sub>2</sub> [mol] consumed per time [s<sup>-1</sup>] 1214 in one litre [L<sup>-1</sup>], but also the change in the concentration of oxygen per second (for any volume 1215 of an ideally closed system). This is ideal for kinetic modeling as it blends with chemical rate 1216 equations where concentrations are typically expressed in mol·L<sup>-1</sup> (Wagner et al. 2011). In 1217 studies of multinuclear cells, such as differentiated skeletal muscle cells, it is easy to determine 1218 1219 the number of nuclei but not the total number of cells. A generalized concept, therefore, is obtained by substituting cells by nuclei as the sample entity. This does not hold, however, for 1220 1221 enucleated platelets.

1222

1223Table 8. Conversion of various units used in respirometry and1224ergometry. e is the number of electrons or reducing equivalents.  $z_B$  is the1225charge number of entity B.

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	//n	

1 Unit	2	x	Multiplication factor	SI-Unit	Note
ng.atom O·s <sup>-1</sup>	(2 e)		0.5	nmol O <sub>2</sub> ·s <sup>-1</sup>	
ng.atom O·min <sup>-1</sup>	(2 e)		8.33	pmol O <sub>2</sub> ·s <sup>-1</sup>	
natom O·min <sup>-1</sup>	(2 e)		8.33	pmol O <sub>2</sub> ·s <sup>-1</sup>	
nmol O <sub>2</sub> ·min <sup>-1</sup>	(4 e)		16.67	pmol O <sub>2</sub> ·s <sup>-1</sup>	
nmol $O_2 \cdot h^{-1}$	(4 e)		0.2778	pmol O <sub>2</sub> ·s <sup>-1</sup>	
mL O <sub>2</sub> ·min <sup>-1</sup> at ST	$\mathbf{PD}^{a}$		0.744	µmol O₂·s <sup>-1</sup>	1
W = J/s at -470 kJ	/mol O <sub>2</sub>		-2.128	µmol O₂·s <sup>-1</sup>	
$mA = mC \cdot s^{-1}$	( <i>z</i> <sub>H+</sub> =1)		10.36	nmol $H^+ \cdot s^{-1}$	2
$mA = mC \cdot s^{-1}$	(z <sub>02</sub> =4)		2.59	nmol O <sub>2</sub> ·s <sup>-1</sup>	2
nmol H <sup>+</sup> ·s <sup>-1</sup>	( <i>z</i> <sub>H+</sub> =1)		0.09649	mA	3
nmol O <sub>2</sub> ·s <sup>-1</sup>	(zo2=4)		0.38594	mA	3

1227

1228	1 At standard temperature and pressure dry (STPD: 0 °C=273.15 K and 1
1229	atm=101.325 kPa=760 mmHg), the molar volume of an ideal gas, $V_{\rm m}$ , and $V_{\rm m,O2}$
1230	is 22.414 and 22.392 L.mol <sup>-1</sup> respectively. Rounded to three decimal places, both
1231	values yield the conversion factor of 0.744. For comparison at NTPD (20 $^{\circ}$ C),
1232	$V_{m,O2}$ is 24.038 L.mol <sup>-1</sup> . Note that the SI standard pressure is 100 kPa.

1233 2 The multiplication factor is  $10^{6}/(z_{\rm B}\cdot F)$ .

1234 3 The multiplication factor is  $z_{\rm B} \cdot F/10^6$ .

1235

# 1236 *4.5. Conversion: oxygen, proton and ATP flux*

1237  $J_{O2,k}$  is coupled in mitochondrial steady states to proton cycling,  $J_{\infty H^+} = J_{H^+,out} = J_{H^+,in}$  (Fig.

1238 2).  $J_{H+,out/n}$  and  $J_{H+,in/n}$  [nmol·s<sup>-1</sup>·L<sup>-1</sup>] are converted into electrical units,  $J_{H+,out/e}$ 

1239  $[mC \cdot s^{-1} \cdot L^{-1} = mA \cdot L^{-1}] = J_{H^+,out/n} [nmol \cdot s^{-1} \cdot L^{-1}] \cdot F [C \cdot mol^{-1}] \cdot 10^{-6}$  (**Table 4**). At a  $J_{H^+,out/J} = J_{H^+,out/n} [nmol \cdot s^{-1} \cdot L^{-1}] \cdot F [C \cdot mol^{-1}] \cdot 10^{-6}$  (**Table 4**).

1240	or $H^+_{out}/O_2$ of 20 ( $H^+_{out}/O=10$ ), a	volume-specific O <sub>2</sub> flux	of 100 nmol·s <sup>-1</sup> ·L <sup>-</sup>	<sup>1</sup> would correspond
------	--	-------------------------------------	---	-------------------------------

1241 to a proton flux of 2,000 nmol 
$$H^+_{out} \cdot s^{-1} \cdot L^{-1}$$
 or volume-specific current of 193 mA·L<sup>-1</sup>.

1242 
$$J_{V,H+out/e} [mA \cdot L^{-1}] = J_{V,H+out/n} \cdot F \cdot 10^{-6} [nmol \cdot s^{-1} \cdot L^{-1} \cdot mC \cdot nmol^{-1}]$$
 (Eq. 3.1)

1243 
$$J_{V,H+out/e} [mA \cdot L^{-1}] = J_{V,O2} \cdot (H^{+}_{out}/O_2) \cdot F \cdot 10^{-6} [mC \cdot s^{-1} \cdot L^{-1} = mA \cdot L^{-1}]$$
(Eq. 3.2)

1244

## 1245 **Table 9. Conversion for units with preservation of numerical values.**

Name	Frequently used unit	Equivalent unit	Note
Volume-specific flux, $J_{V,O2}$	pmol·s <sup>-1</sup> ·mL <sup>-1</sup> mmol·s <sup>-1</sup> ·L <sup>-1</sup>	nmol·s <sup>-1</sup> ·L <sup>-1</sup> mol·s <sup>-1</sup> ·m <sup>-3</sup>	1
Cell-specific flow, $I_{02}$	pmol·s <sup>-1</sup> ·10 <sup>-6</sup> cells	amol·s <sup>-1</sup> ·cell <sup>-1</sup>	2
-	pmol·s <sup>-1</sup> ·10 <sup>-9</sup> cells	zmol·s <sup>-1</sup> ·cell <sup>-1</sup>	3
Cell number concentration, $C_{Nce}$	10 <sup>6</sup> cells⋅mL <sup>-1</sup>	$10^9$ cells·L <sup>-1</sup>	
Mitochondrial protein concentration, $C_{\text{mte}}$	0.1 mg·mL <sup>-1</sup>	$0.1 \text{ g} \cdot \text{L}^{-1}$	
Mass-specific flux, $J_{m,O2}$	pmol·s <sup>-1</sup> ·mg <sup>-1</sup>	nmol·s <sup>-1</sup> ·g <sup>-1</sup>	4
Catabolic power, $P_{k,O2}$	µW·10 <sup>-6</sup> cells	pW·cell <sup>-1</sup>	1
Volume	1,000 L	m <sup>3</sup> (1,000 kg)	
	L	$dm^3$ (kg)	
	mL	$cm^{3}(g)$	
	μL	$mm^3$ (mg)	
	fL	$\mu m^3$ (pg)	
Amount of substance concentration	$M = mol \cdot L^{-1}$	mol·dm <sup>-3</sup>	

1247 1 pmol: picomole =  $10^{-12}$  mol

1248 2 amol: attomole =  $10^{-18}$  mol 1249 3 zmol: zeptomole =  $10^{-21}$  mol

1249 3 zmol: zeptomole =  $10^{-21}$  mol 1250 4 nmol: nanomole =  $10^{-9}$  mol

1250 4 nm 1251

ET capacity in various human cell types including HEK 293, primary HUVEC and fibroblasts 1252 ranges from 50 to 180 amol·s<sup>-1</sup>·cell<sup>-1</sup>, measured in intact cells in the noncoupled state (see 1253 Gnaiger 2014). At 100 amol·s<sup>-1</sup>·cell<sup>-1</sup> corrected for ROX (corresponding to a catabolic power 1254 of -48 pW·cell<sup>-1</sup>), the current across the mt-membranes,  $I_e$ , approximates 193 pA·cell<sup>-1</sup> or 0.2 1255 1256 nA per cell. See Rich (2003) for an extension of quantitative bioenergetics from the molecular to the human scale, with a transmembrane proton flux equivalent to 520 A in an adult at a 1257 catabolic power of -110 W. Modelling approaches illustrate the link between proton motive 1258 1259 force and currents (Willis et al. 2016). For NADH- and succinate-linked respiration, the mechanistic P»/O<sub>2</sub> ratio (referring to the full 4 electron reduction of O<sub>2</sub>) is calculated at 20/3.7 and 12/3.7, respectively (Eq. 4) equal to 5.4 and 3.3. The classical P»/O ratios (referring to the lectron reduction of 0.5 O<sub>2</sub>) are 2.7 and 1.6 (Watt *et al.* 2010), in direct agreement with the measured P»/O ratio for succinate of  $1.58 \pm 0.02$  (Gnaiger *et al.* 2000; for detailed reviews see Wikström and Hummer 2012; Sazanov 2015),

1267

$$P \gg O_2 = (H_{out}^+ O_2) / (H_{in}^+ P \gg)$$
 (Eq. 4)

1266 In summary (**Fig. 1**),

- $J_{V,P*}[nmol \cdot s^{-1} \cdot L^{-1}] = J_{V,O2} \cdot (H^{+}_{out}/O_2) / (H^{+}_{in}/P*)$ (Eq. 5.1)
- 1268  $J_{V,P*}$  [nmol·s<sup>-1</sup>·L<sup>-1</sup>] =  $J_{V,O2}$ ·(P\*/O<sub>2</sub>) (Eq. 5.2)

We consider isolated mitochondria as powerhouses and proton pumps as molecular machines 1269 1270 to relate experimental results to energy metabolism of the intact cell. The cellular P»/O2 based on oxidation of glycogen is increased by the glycolytic (fermentative) substrate-level 1271 1272 phosphorylation of 3 P»/Glyc, i.e., 0.5 mol P» for each mol O2 consumed in the complete oxidation of a mol glycosyl unit (Glyc). Adding 0.5 to the mitochondrial P»/O2 ratio of 5.4 1273 yields a bioenergetic cell physiological P»/O2 ratio close to 6. Two NADH equivalents are 1274 formed during glycolysis and transported from the cytosol into the mitochondrial matrix, either 1275 1276 by the malate-aspartate shuttle or by the glycerophosphate shuttle resulting in different 1277 theoretical yield of ATP generated by mitochondria, the energetic cost of which potentially 1278 must be taken into account. Considering also substrate-level phosphorylation in the TCA cycle, 1279 this high P»/O<sub>2</sub> ratio not only reflects proton translocation and OXPHOS studied in isolation, 1280 but integrates mitochondrial physiology with energy transformation in the living cell (Gnaiger 1993a). 1281

1282

#### 1283 **5.** Conclusions

1284 MitoEAGLE can serve as a gateway to better diagnose mitochondrial respiratory defects 1285 linked to genetic variation, age-related health risks, sex-specific mitochondrial performance, lifestyle with its effects on degenerative diseases, and thermal and chemical environment. The present recommendations on coupling control states and rates, linked to the concept of the protonmotive force (Part 1) will be extended in a series of reports on pathway control of mitochondrial respiration, respiratory states in intact cells, and harmonization of experimental procedures.

1291

## 1292 Box 5: Mitochondrial and cell respiration

1293 Mitochondrial and cell respiration is the process of highly exergonic and exothermic energy transformation in which scalar redox reactions are coupled to vectorial ion translocation across 1294 1295 a semipermeable membrane, which separates the small volume of a bacterial cell or 1296 mitochondrion from the larger volume of its surroundings. The electrochemical exergy can be partially conserved in the phosphorylation of ADP to ATP or in ion pumping, or dissipated in 1297 1298 an electrochemical short-circuit. Respiration is thus clearly distinguished from fermentation as the counterpart of cellular core energy metabolism. Respiration is separated in mitochondrial 1299 preparations from the partial contribution of fermentative pathways of the intact cell. According 1300 1301 to this definition, residual oxygen consumption, as measured after inhibition of mitochondrial electron transfer, does not belong to the class of catabolic reactions and is, therefore, subtracted 1302 from total oxygen consumption to obtain baseline-corrected respiration. 1303

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The optimal choice for expressing mitochondrial and cell respiration (**Box 5**) as  $O_2$  flow per biological system, and normalization for specific tissue-markers (volume, mass, protein) and mitochondrial markers (volume, protein, content, mtDNA, activity of marker enzymes, respiratory reference state) is guided by the scientific question. Interpretation of the obtained data depends critically on appropriate normalization, and therefore reporting rates merely as nmol·s<sup>-1</sup> is discouraged, since it restricts the analysis to intra-experimental comparison of relative (qualitative) differences. Expressing  $O_2$  consumption per cell may not be possible when

dealing with tissues. For studies with mitochondrial preparations, we recommend that 1312 1313 normalizations be provided as far as possible: (1) on a per cell basis as  $O_2$  flow (a biophysical 1314 normalization); (2) per g cell or tissue protein, or per cell or tissue mass as mass-specific  $O_2$ flux (a cellular normalization); and (3) per mitochondrial marker as mt-specific flux (a 1315 1316 mitochondrial normalization). With information on cell size and the use of multiple normalizations, maximum potential information is available (Renner et al. 2003; Wagner et al. 1317 1318 2011; Gnaiger 2014). When using isolated mitochondria, mitochondrial protein is a frequently applied mitochondrial marker, the use of which is basically restricted to isolated mitochondria. 1319 Mitochondrial markers, such as citrate synthase activity as an enzymatic matrix marker, provide 1320 1321 a link to the tissue of origin on the basis of calculating the mitochondrial yield, *i.e.*, the fraction 1322 of mitochondrial marker obtained from a unit mass of tissue.

1323

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